

# Diffusion-trapping models of protein receptor trafficking along spiny dendrites

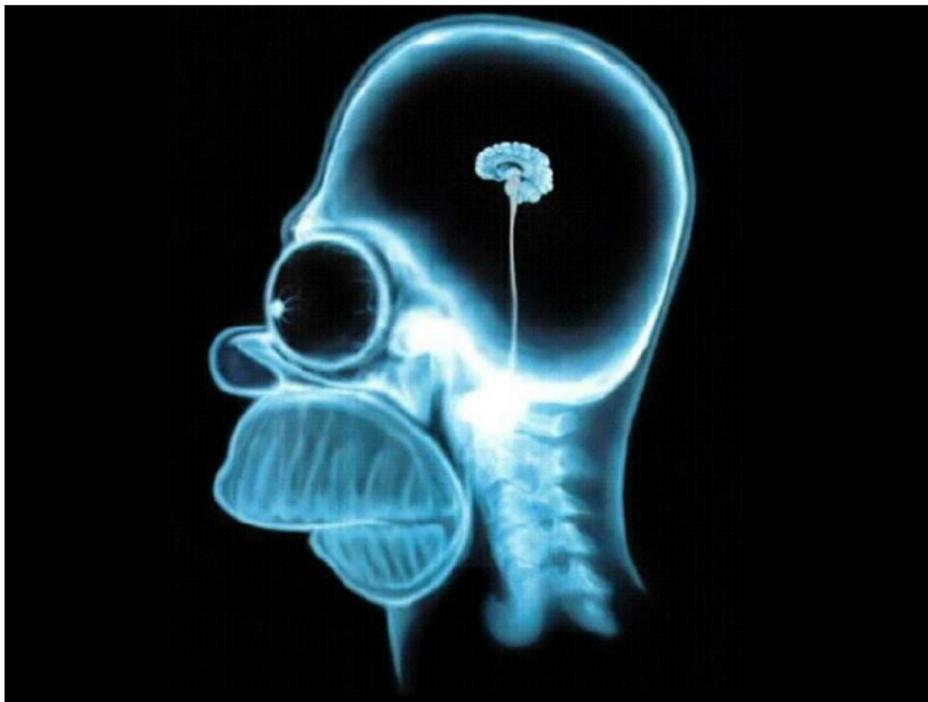
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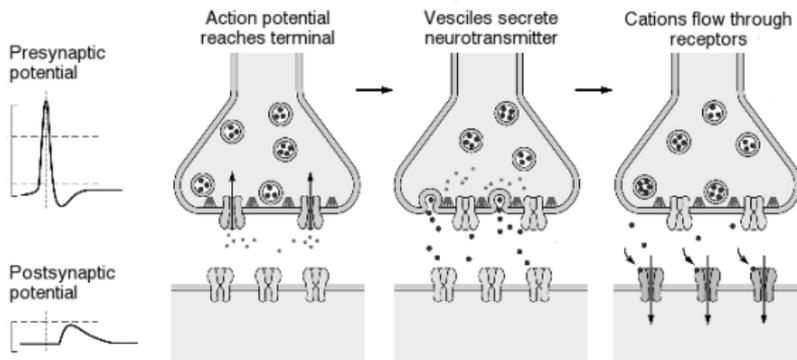
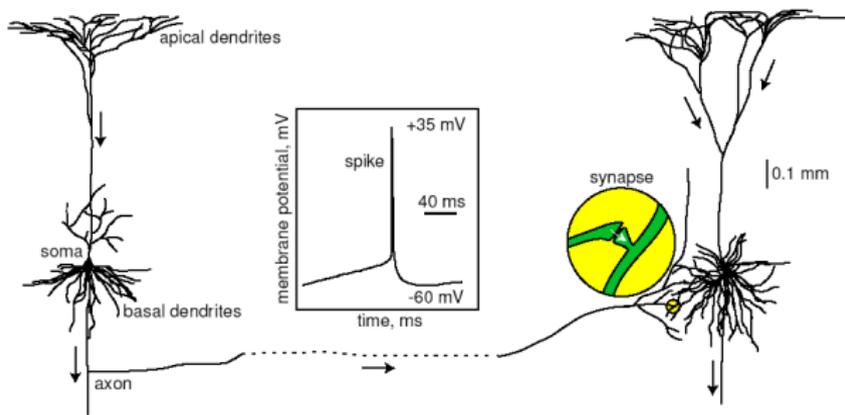
<sup>2</sup>Department of Mathematics, University of British Columbia  
Vancouver, B.C., Canada

June 25, 2008

# The amazing brain

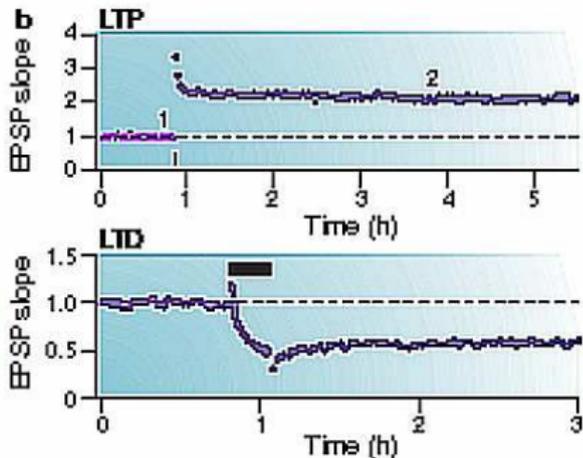
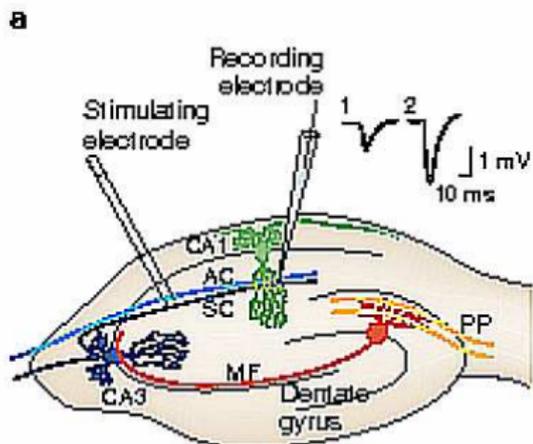


# Neurons communicate at synapses



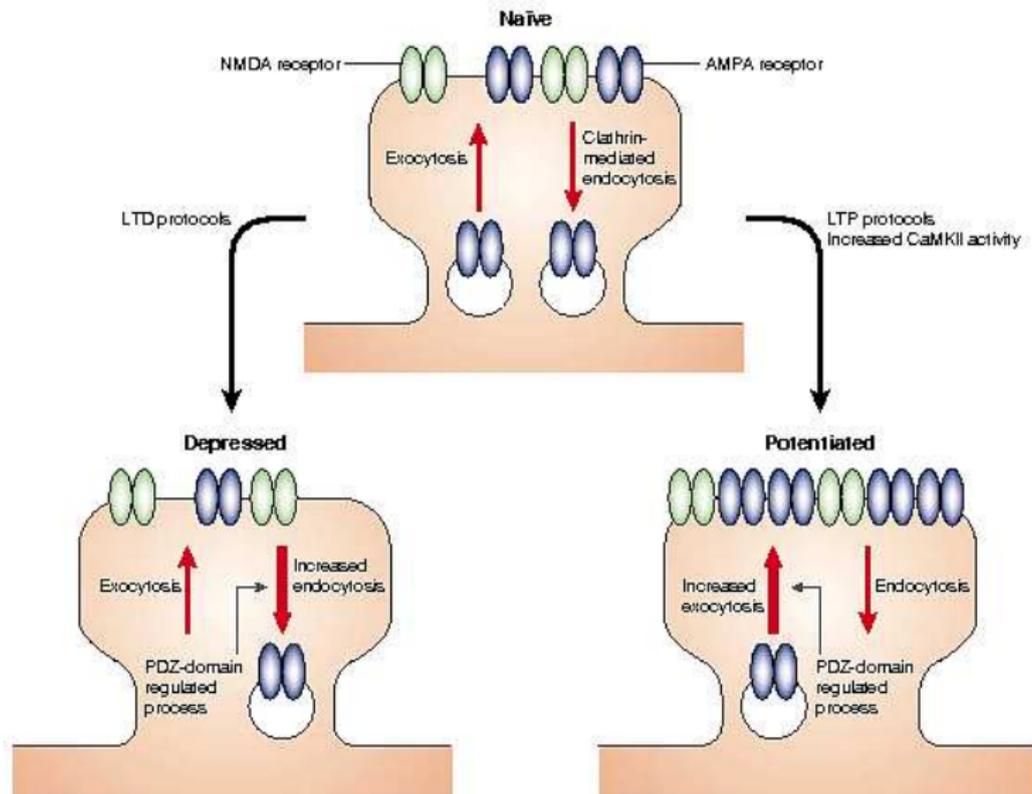
Kandel, Schwartz & Jessel (2000)

# Synapses can “learn”

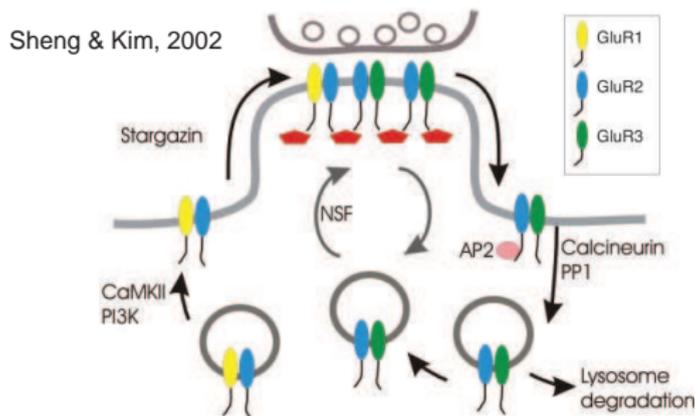


Collingridge et al., *Nat. Rev. Neurosci.* (2004)

# Synapses “learn” by regulating receptor numbers

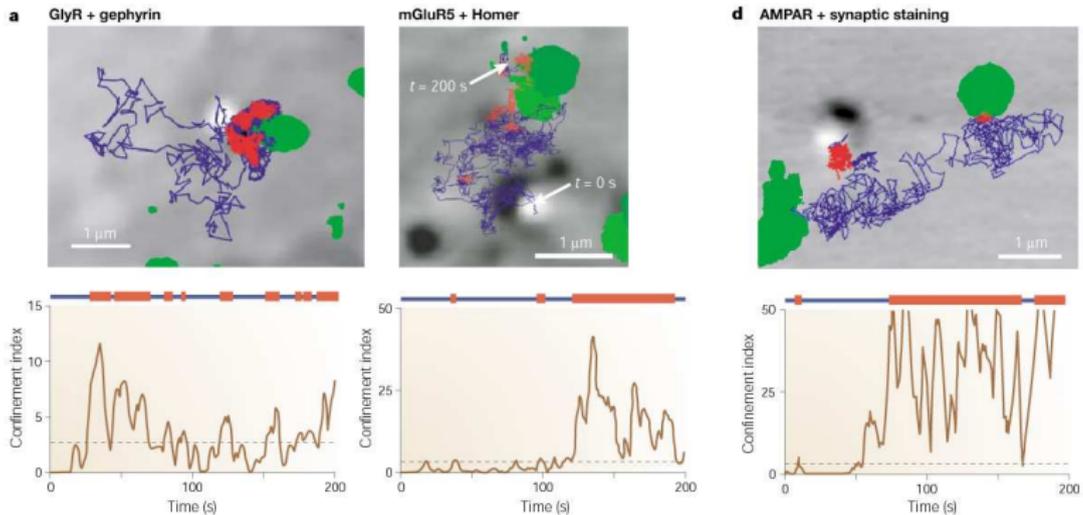


# Receptor trafficking at synapses



- constitutively recycled with intracellular stores
  - AMPA receptors turned over in 10-30 mins (or 16 hrs?)
- immobilized by scaffolding proteins in synapse
- **diffuse** laterally within membrane

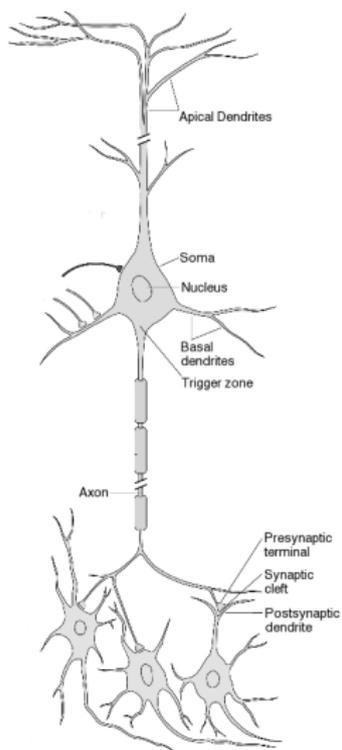
# Receptors diffuse laterally between synapses



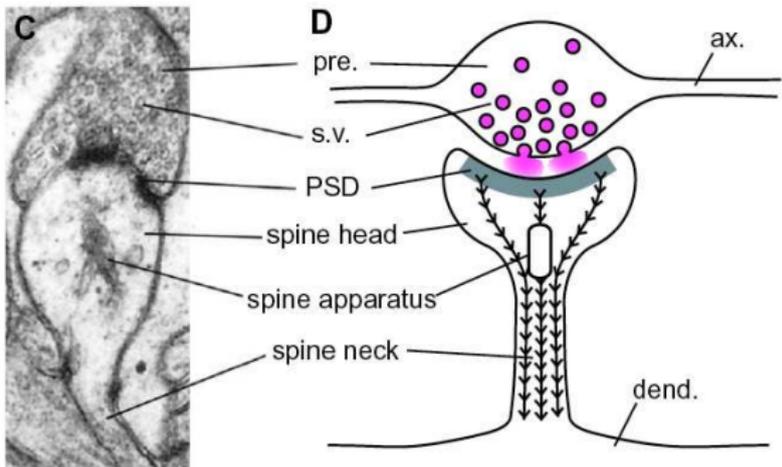
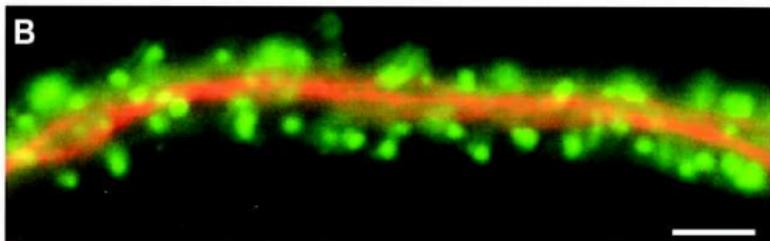
Triller & Choquet, *Nat. Rev. Neurosci.* (2003)

How are receptors transported to synapses?

# Synapses located in dendritic spines

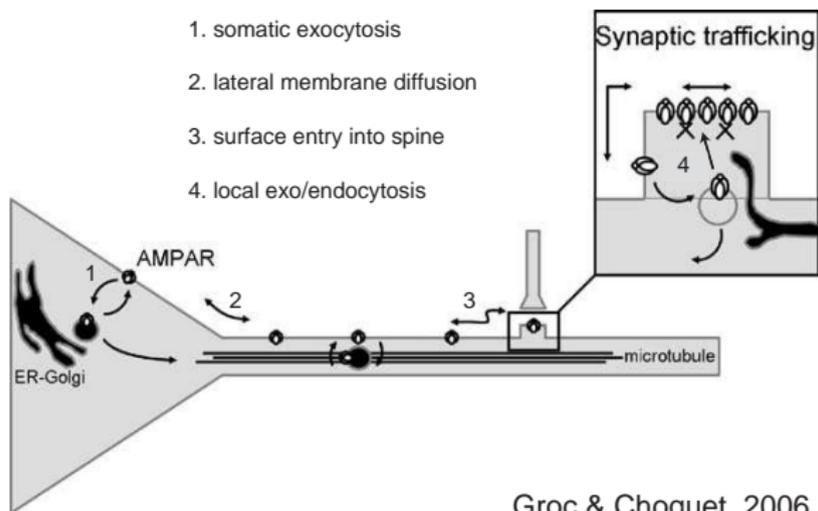


Kandel, Schwartz & Jessel (2000)



Matus, *Science* (2000)

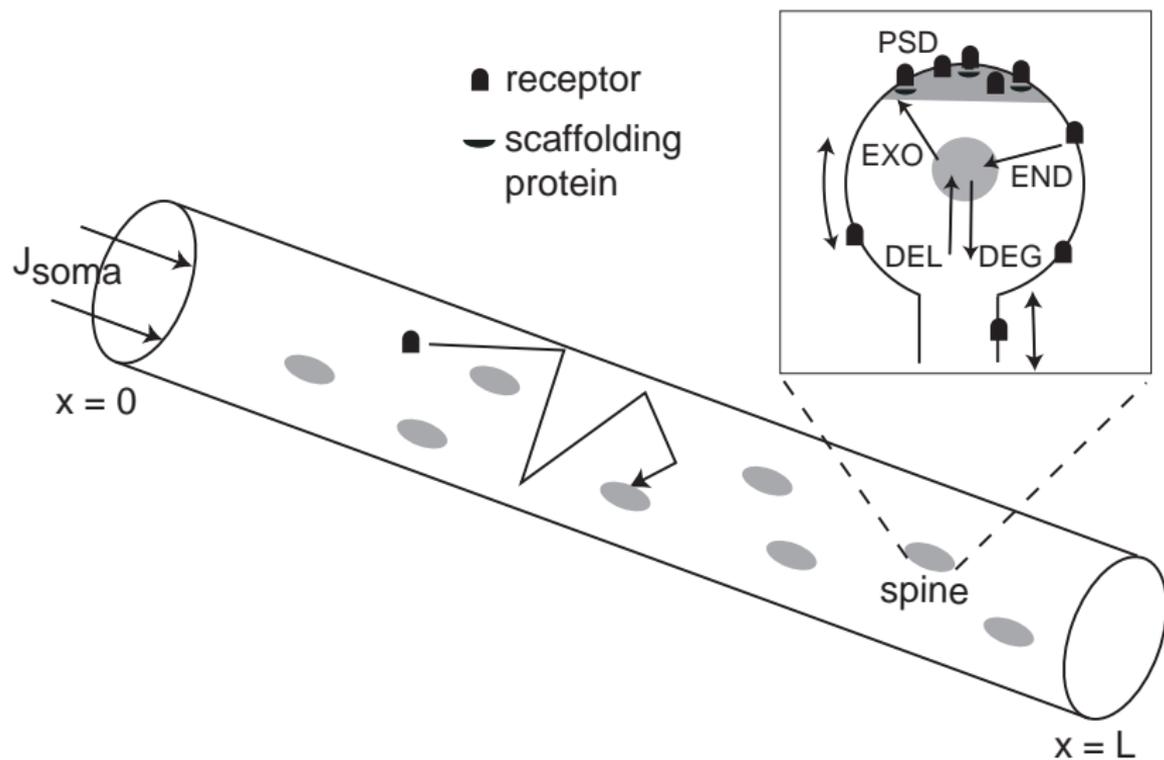
# Long-range transport of receptors along spiny dendrite



- motor transport along microtubules
- **diffusion** within dendritic membrane? (Adesnik et al., 2005)

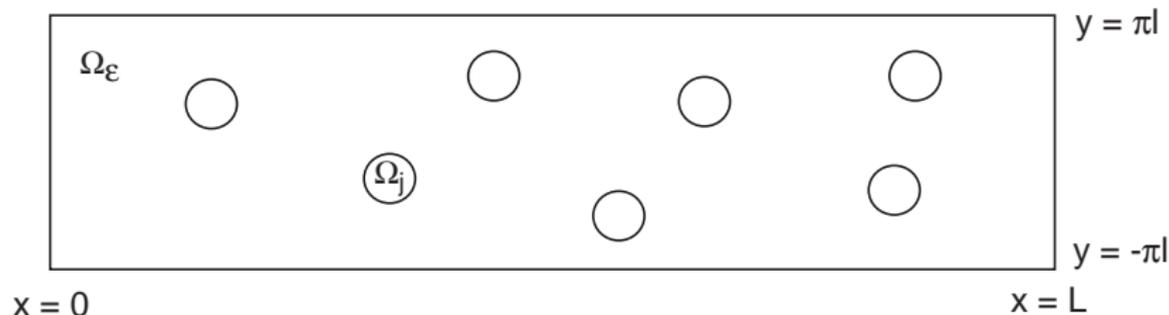
How should we model diffusion-trapping of receptors?

# Treat dendritic membrane as cylinder with holes



# Diffusion equation on dendritic membrane

$$\frac{\partial U}{\partial t} = D \nabla^2 U \quad \text{on } \Omega_\varepsilon$$



- $U$  = receptor concentration
- $\Omega_\varepsilon$  is rectangle  $(0, L) \times (-\pi l, \pi l)$  minus the holes

$$\Omega_j = \{\mathbf{r} \in \Omega_0 \mid |\mathbf{r} - \mathbf{r}_j| \leq \varepsilon \rho\}, \quad j = 1, \dots, N$$

# Boundary conditions

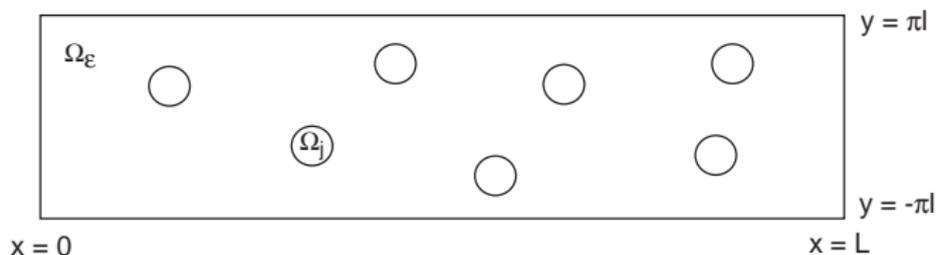
- Periodic bcs at  $y = \pm\pi l$
- No-flux bc at  $x = L$ , and at  $x = 0$

$$-D \frac{\partial U}{\partial x} = J_{soma} = \frac{\sigma}{2\pi l}$$

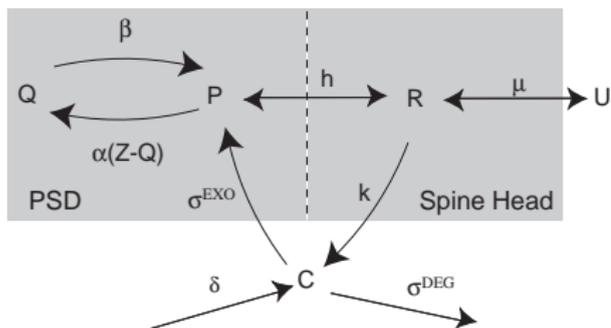
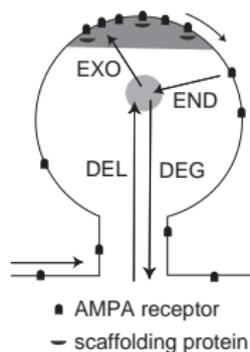
- bcs at the holes:

$$-\varepsilon D \frac{\partial U}{\partial \mathbf{n}}(\mathbf{r}, t) = \frac{\mu_j}{2\pi\rho} (U(\mathbf{r}, t) - R_j), \quad \mathbf{r} \in \partial\Omega_j$$

- $\mu_j$  = spine neck hopping rate
- $R_j$  = receptor concentration on surface of  $j$ th spine



# Treat each spine as having 3 compartments



- P, Q:** unbound, bound receptor concentrations in PSD  
**R, U:** free receptor concentrations in spine head, dendrite  
**C:** number of intracellular receptors  
**k,  $\sigma^{\text{EXO}}$ :** rates of endocytosis, exocytosis  
 **$\sigma^{\text{DEG}}$ ,  $\delta$ :** rates of degradation, intracellular delivery  
**h,  $\mu$ :** hopping rates across boundary of PSD, spine neck  
 **$\alpha(\text{Z-Q})$ :** rate of binding to scaffolding (Z = scaffolding concentration)  
 **$\beta$ :** rate of unbinding from scaffolding

# Steady-state solution

- All steady-state concentrations at  $j$ th spine depend on the mean value of  $U$  on  $\partial\Omega_j$ :

$$U_j = \frac{1}{2\pi\epsilon\rho} \int_{\partial\Omega_j} U(\mathbf{r}) d\mathbf{r}$$

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- $U_j$ 's are determined by solving  $\nabla^2 U = 0$  in  $\Omega_\epsilon$  with bcs
- But this is **hard** because of bcs at the holes!

$$-\epsilon D \frac{\partial U}{\partial \mathbf{n}}(\mathbf{r}) = \frac{\mu_j}{2\pi\rho} (U(\mathbf{r}) - R_j), \quad \mathbf{r} \in \partial\Omega_j$$

## Three steps for finding approximate steady-state solution

- 1 Solve assuming  $U = U_j$  on the boundary of  $j$ th hole

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  - **Singular perturbation:** match logarithmic solutions in each inner region

$$|\mathbf{r} - \mathbf{r}_j| = \mathcal{O}(\varepsilon)$$

with Green's function singularities in outer region

$$|\mathbf{r} - \mathbf{r}_j| = \mathcal{O}(1) \text{ for all } j$$

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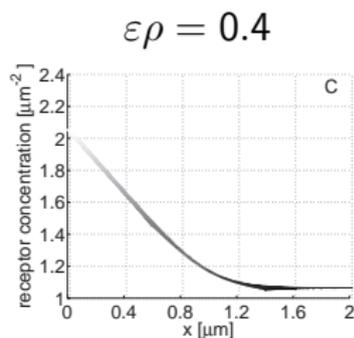
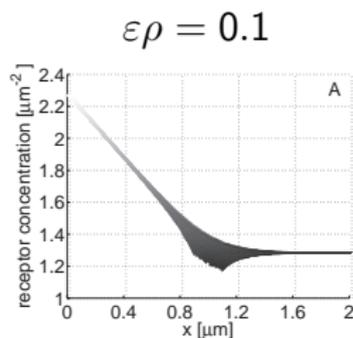
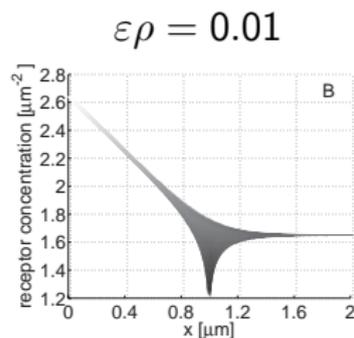
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- 3 Conservation condition gives  $(N + 1)$ th equation

$$\sigma = \sum \hat{\mu}_j (U_j - \hat{R}_j)$$

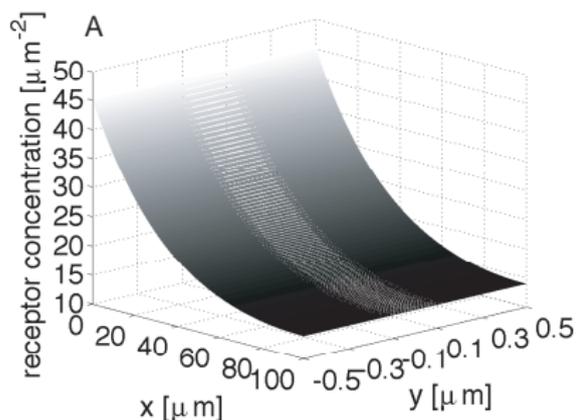
# Effect of $\varepsilon\rho$ on solution



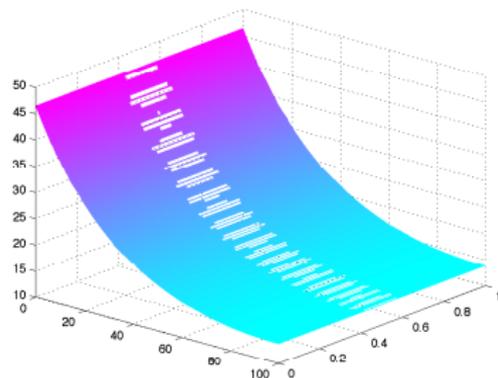
- Dendrite  $2\mu\text{m}$  long, circumference  $1\mu\text{m}$
- One spine at  $\mathbf{r} = (1, 0.5)$
- Numerical solutions look similar

# Comparison of dendritic receptor concentration

perturbation solution



numerical solution



- Dendrite  $100\mu\text{m}$  long, circumference  $1\mu\text{m}$ ,  $\epsilon\rho = 0.1\mu\text{m}$
- 100 identical spines spaced  $1\mu\text{m}$  apart, all in a row
- Solutions are almost identical!
- Similar results if spines are not identical, not in a row

Can we make things simpler?

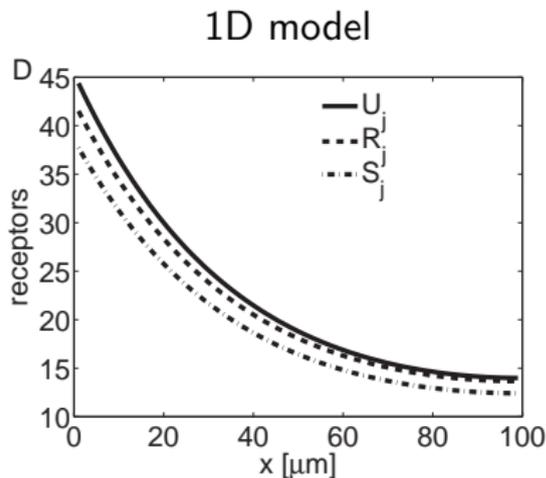
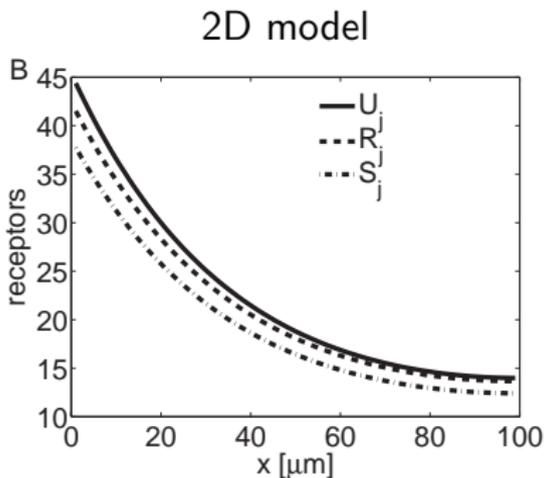
## 2D model well-approximated by 1D model

When the aspect ratio  $L/l \gg 1$ , we can approximate 2D model by the following 1D model

$$\frac{\partial U}{\partial t} = D \frac{\partial^2 U}{\partial x^2} - \sum_{j=1}^N \delta(x - x_j) \mu_j (U_j - R_j)$$

$$-D \left. \frac{\partial U}{\partial x} \right|_{x=0} = J_{\text{soma}}, \quad \left. \frac{\partial U}{\partial x} \right|_{x=L} = 0.$$

# Comparison of models



- 2D model as before
  - Dendrite  $100\mu\text{m}$  long, circumference  $1\mu\text{m}$ ,  $\epsilon\rho = 0.1\mu\text{m}$
  - 100 identical spines spaced  $1\mu\text{m}$  apart, all in a row
- 1D model use same parameters when relevant
- Solutions are almost identical!

Can we make things even simpler?

# Treat spine population as continuous density

If spines are sufficiently dense, treat sum of delta functions as a density  $\eta$

$$\frac{\partial U}{\partial t} = D \frac{\partial^2 U}{\partial x^2} - \eta(x)\mu(x)(U - R)$$
$$-D \left. \frac{\partial U}{\partial x} \right|_{x=0} = J_{\text{soma}}, \quad \left. \frac{\partial U}{\partial x} \right|_{x=L} = 0.$$

# Steady-state solution for identical spines: “cable” equation

- Assume all parameters are  $x$ -independent, then get “cable” equation for receptor trafficking

$$\frac{d^2 U}{dx^2} - \Lambda^2 U = -\Lambda^2 \hat{R}$$

$$\Lambda = \sqrt{\frac{\eta \hat{\mu}}{D}} \text{ is length-scale of diffusive coupling}$$

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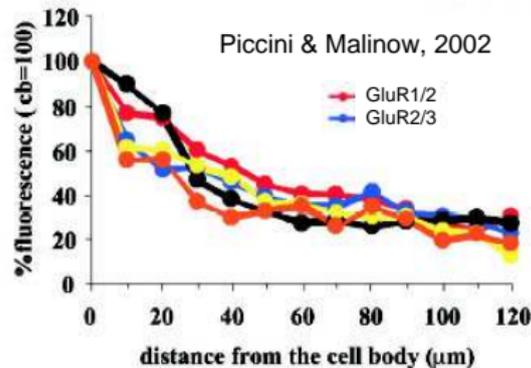
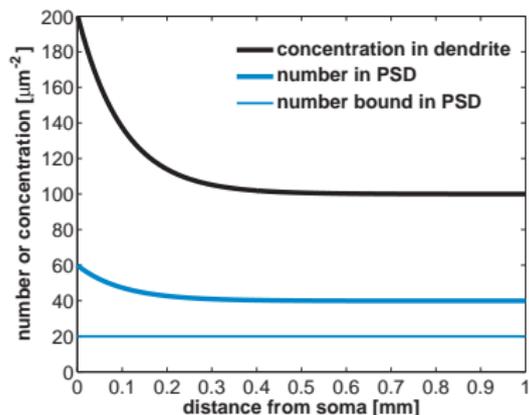
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$$\Lambda = \sqrt{\frac{\eta \hat{\mu}}{D}} \text{ is length-scale of diffusive coupling}$$

- Solve using Green’s function methods

$$U(x) = \frac{J_{\text{soma}}}{D} \frac{\cosh(\Lambda(x - L))}{\Lambda \sinh(\Lambda L)} + \hat{R}$$

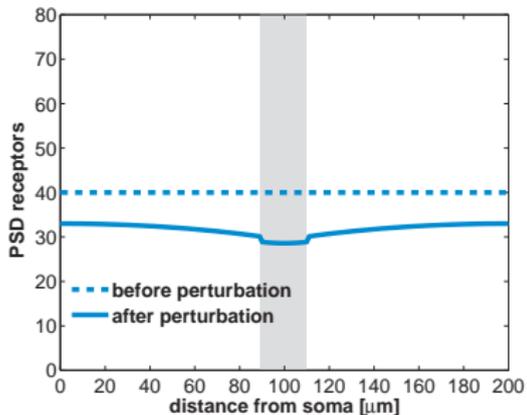
# Steady-state receptor concentrations for identical spines



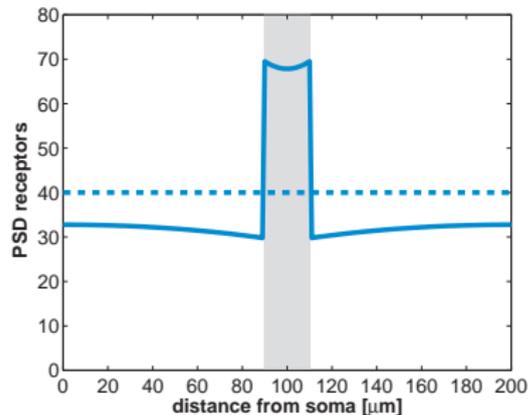
- Dendrite 1 mm long
- 1,000 identical spines spaced  $1\mu\text{m}$  apart
- Two sources of receptors
  - at soma
  - local intracellular delivery

# Consequences of diffusive coupling

10-fold reduction in  
rate of exocytosis  
in gray region

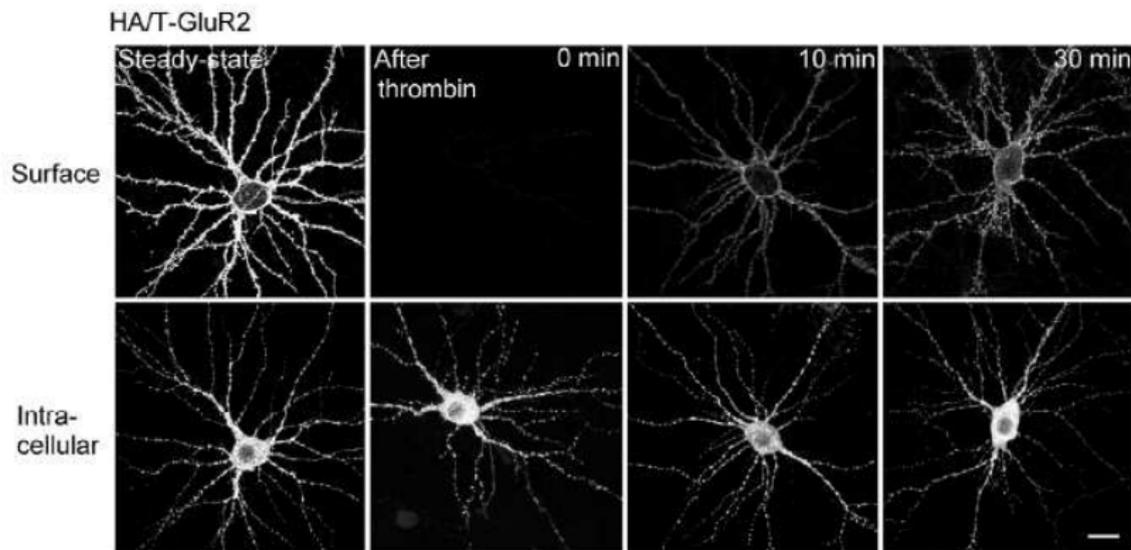


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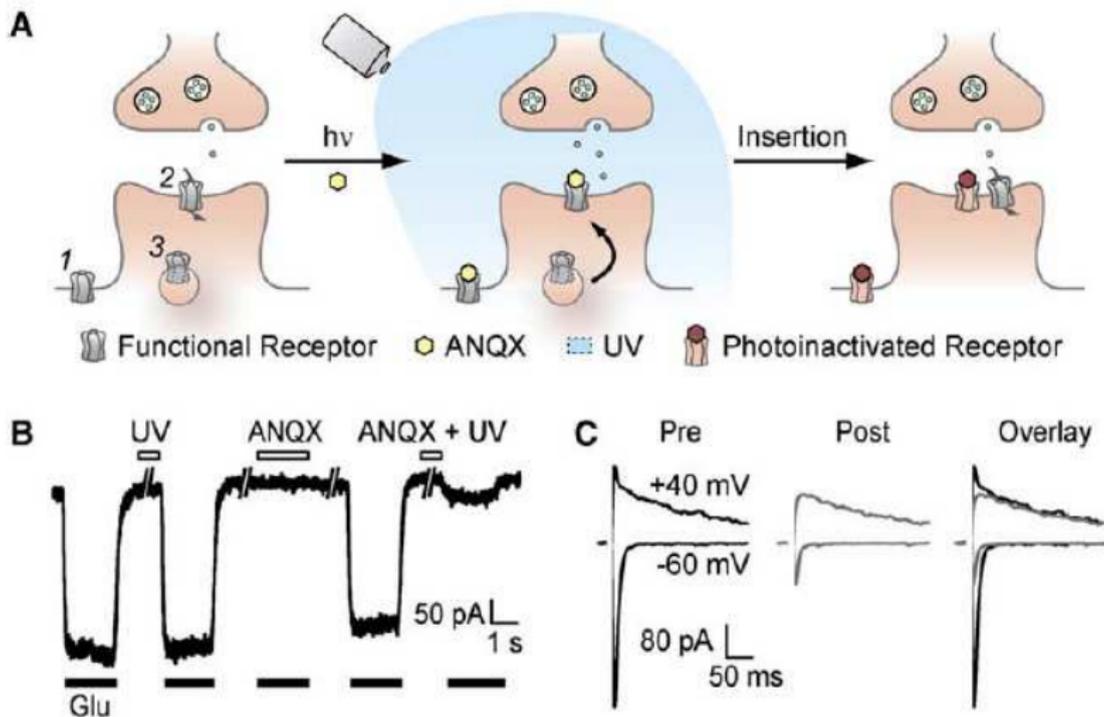
Steady-state is nice...  
...but what about time-dependent phenomena?

# AMPA receptor recycling via thrombin cleavage

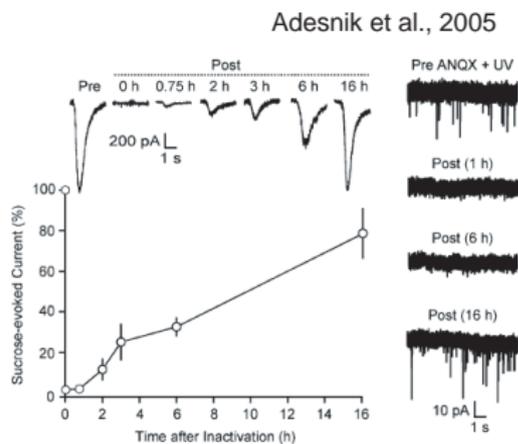
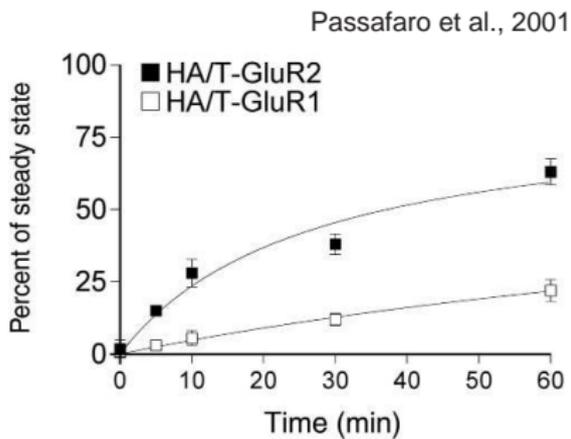


Passafaro et al., *Nat. Neurosci.* (2001)

# AMPA receptor recycling via photoinactivation

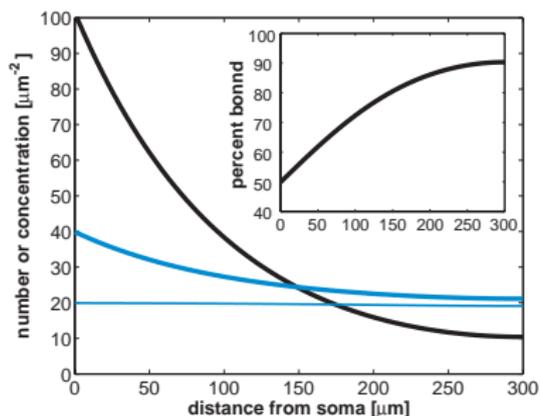


# Fast or slow recycling of AMPA receptors?



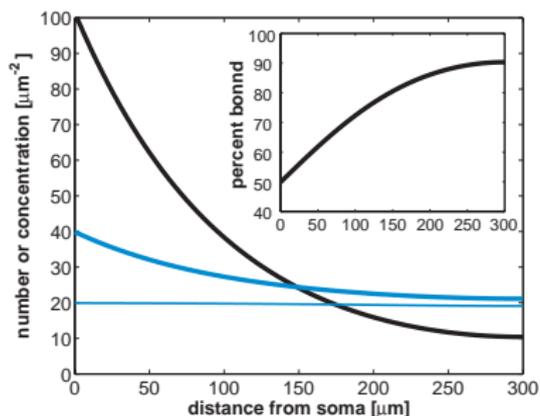
# Simulation of photoinactivation of AMPA receptors

- No intracellular delivery but source at soma
- In steady-state  $t < 0$
- At  $t = 0$  all surface AMPA receptors instantaneously “inactivated”



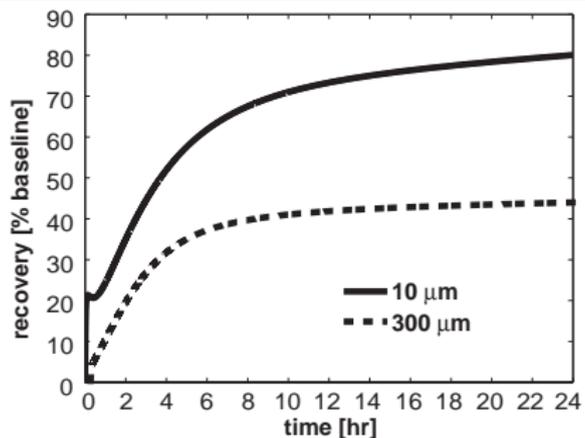
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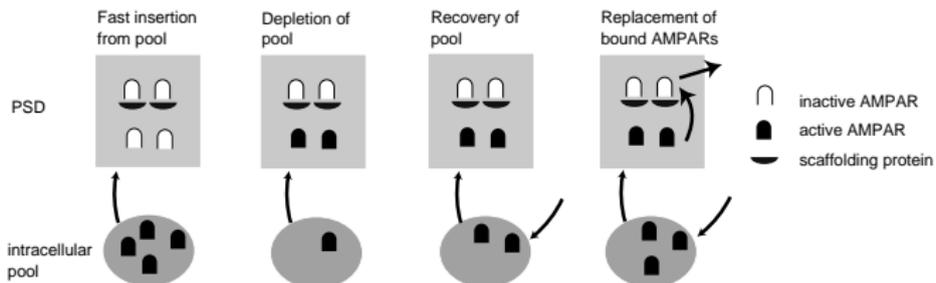


- Rates of exo/endocytosis are **fast** (10-30 mins)

# Rate of recycling depends on distance from soma



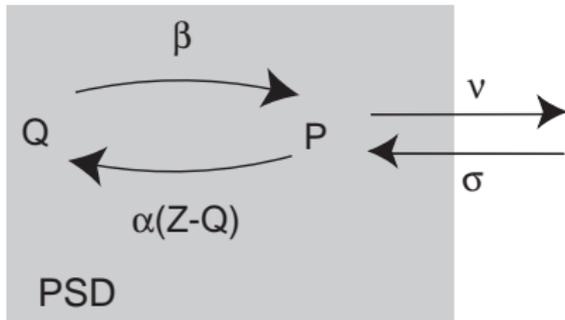
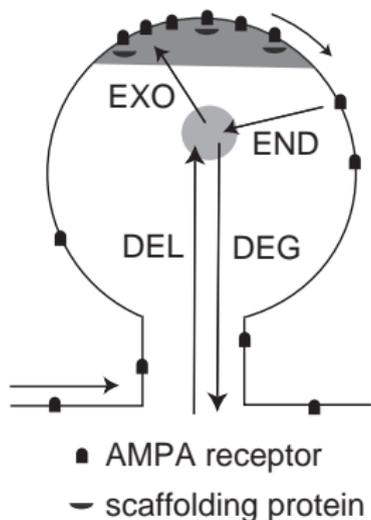
- Fast exo/endocytosis consistent with slow recycling
- There are many time scales!



# Future directions

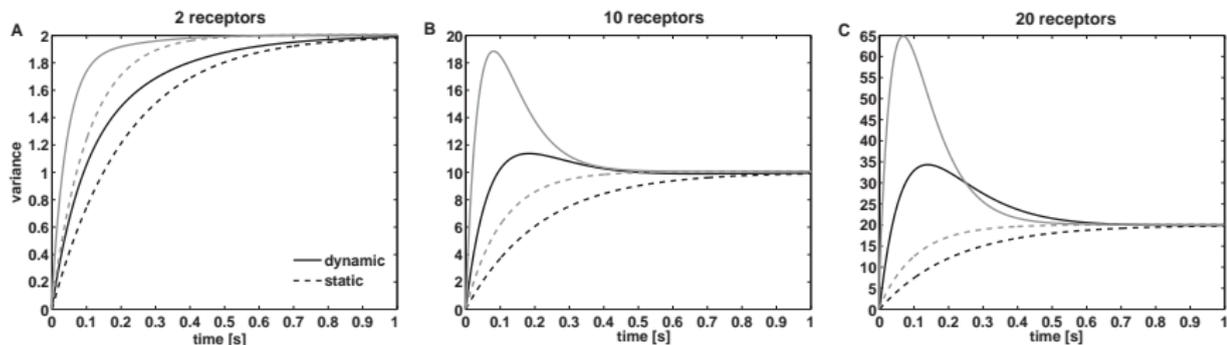
- Models with many kinds of receptors (AMPA, NMDA, kainate, etc.)
- Models with receptor function, electrophysiology
- Computational learning rules (e.g., STDP)
- Role of AMPA receptor trafficking in Alzheimer's disease
- **Stochastic models**

# Intrinsic vs. extrinsic noise of synaptic trafficking



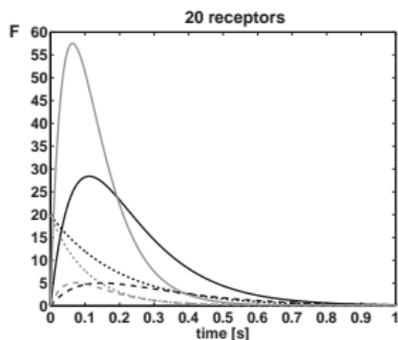
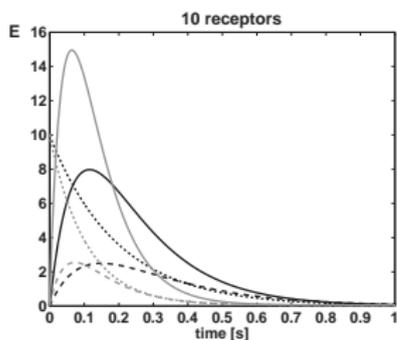
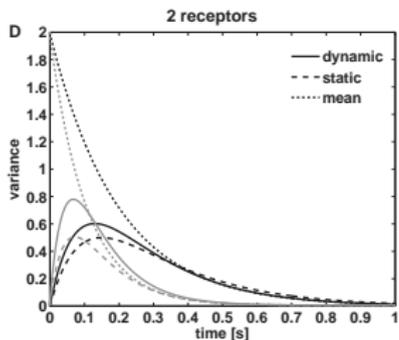
- intrinsic noise: e.g., binding/unbinding
- extrinsic noise: e.g., fluctuating gate

# Time-course of variance during FRAP



- black: with binding
- gray: no binding

# Time-course of variance during Inverse FRAP



- black: with binding
- gray: no binding