

Multiple spatial scales of AMPA receptor trafficking

From synapse to spiny dendrite

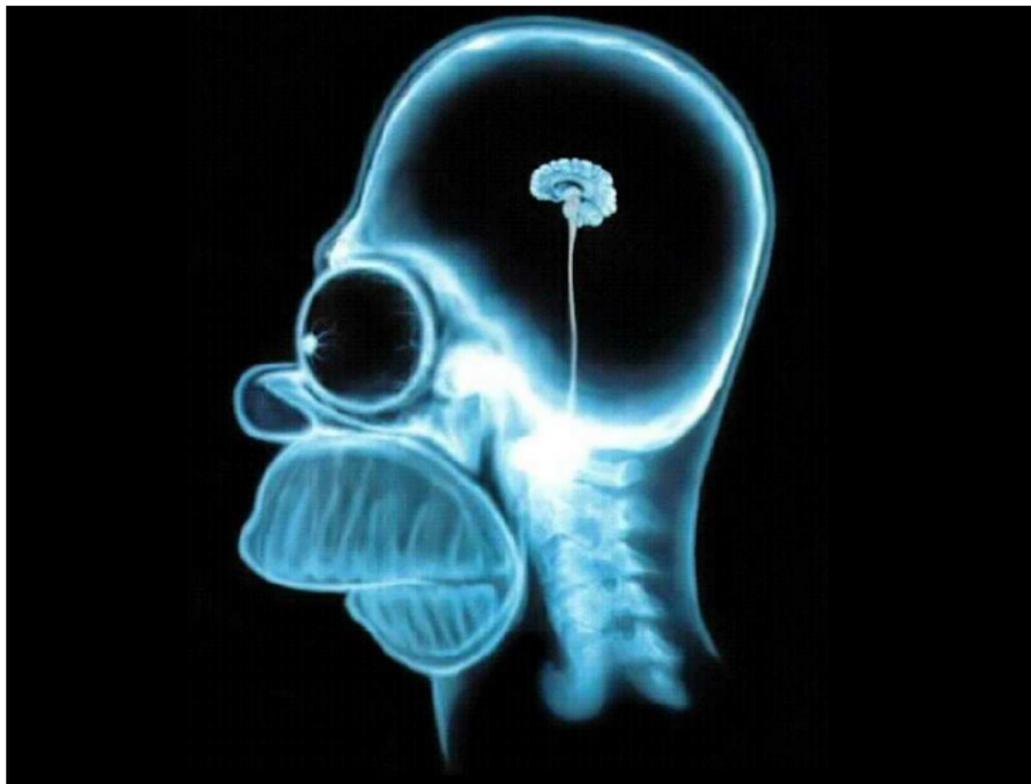
Paul Bressloff Berton Earnshaw

Department of Mathematics
University of Utah

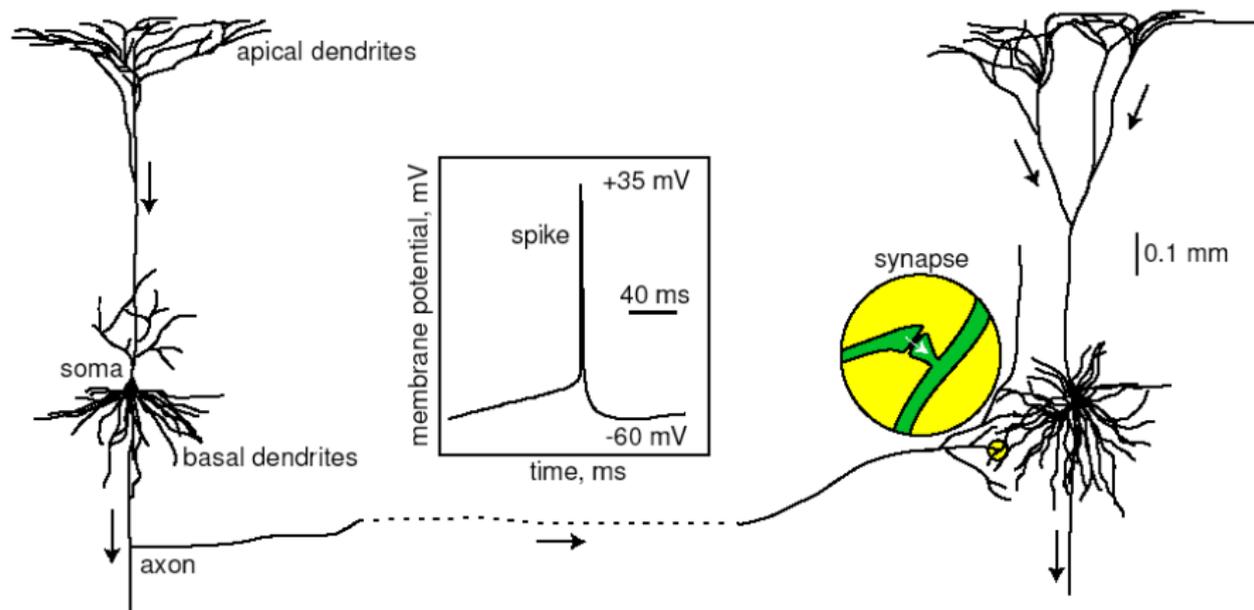
March 26, 2009



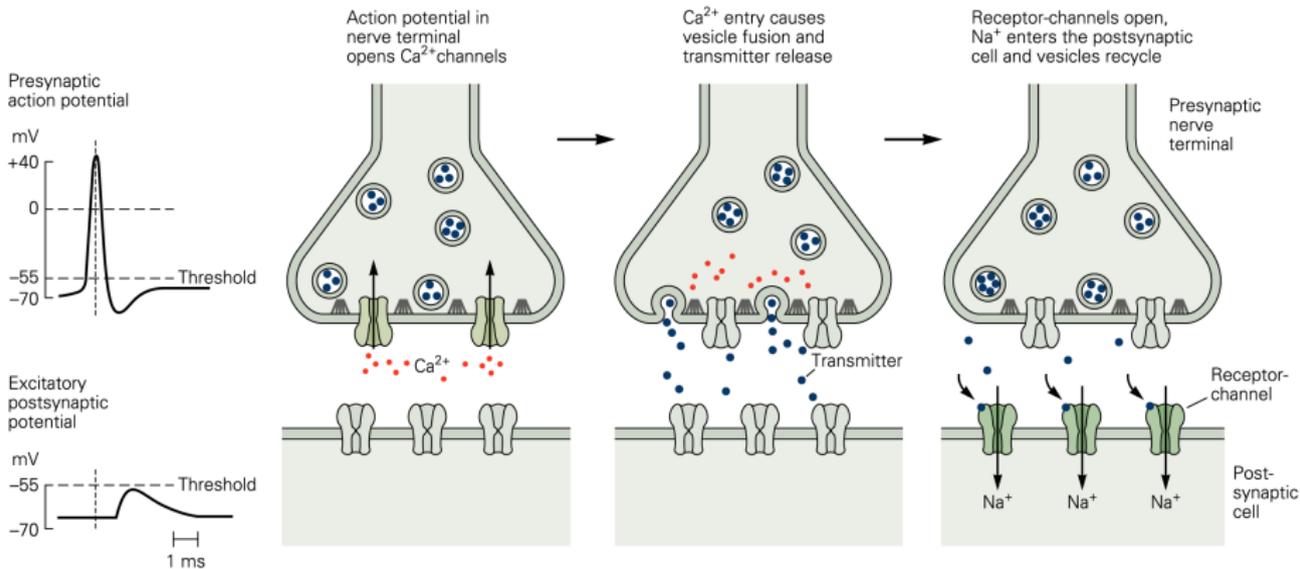
The amazing brain



Neurons communicate at synapses

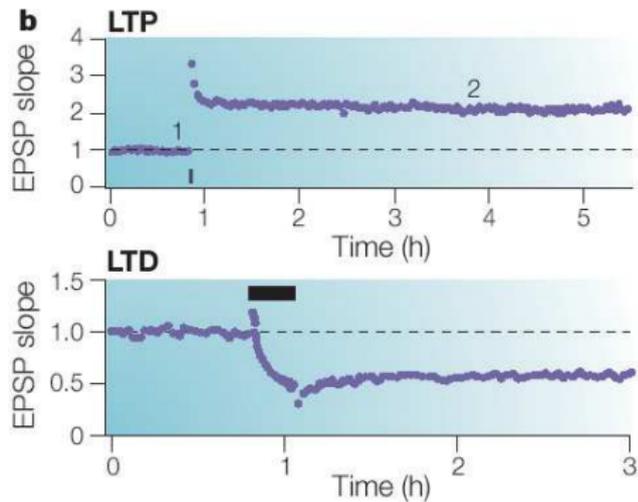
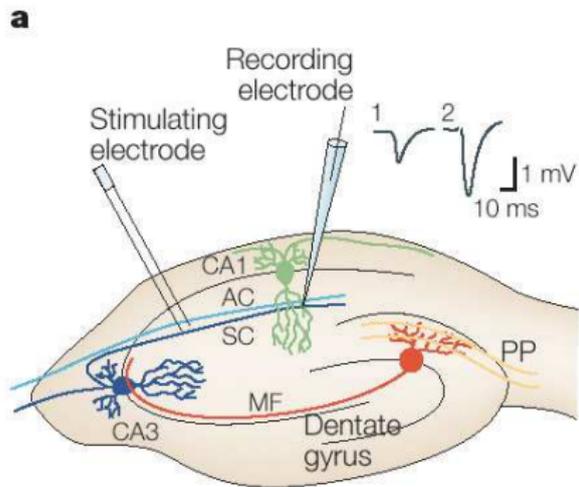


Communication at a synapse



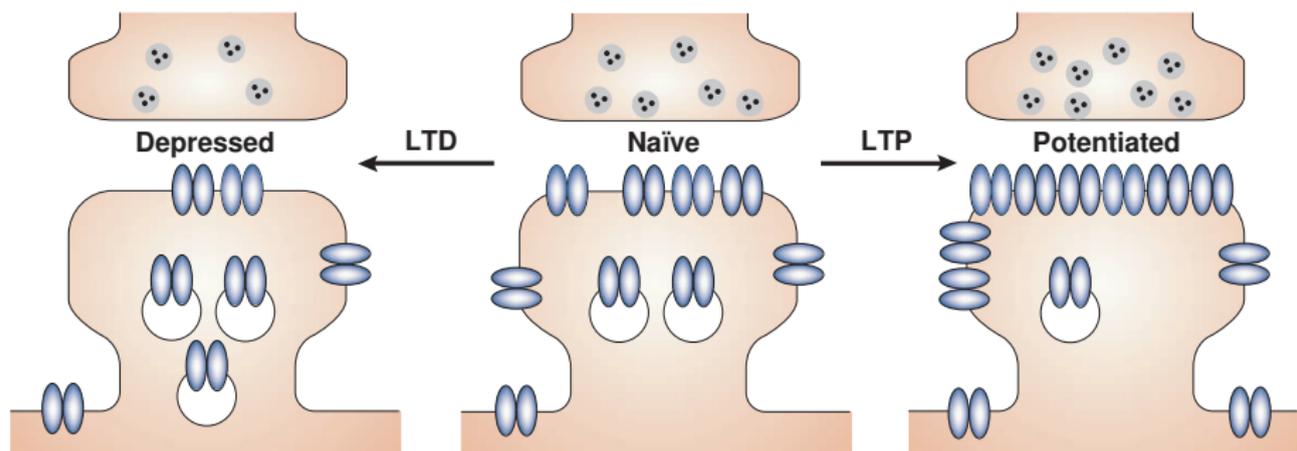
Kandel, Schwartz & Jessel (2000)

Synapses can “learn”

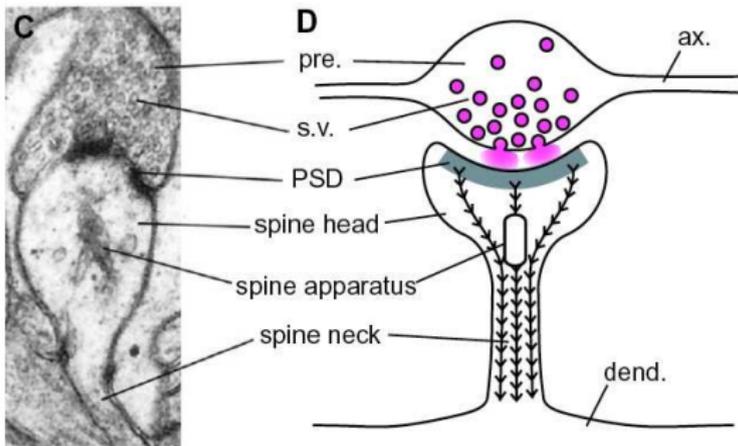
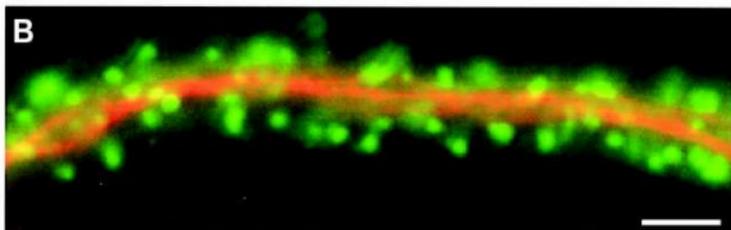


Collingridge et al., *Nat Rev Neurosci* (2004)

Synapses “learn” by regulating receptor numbers

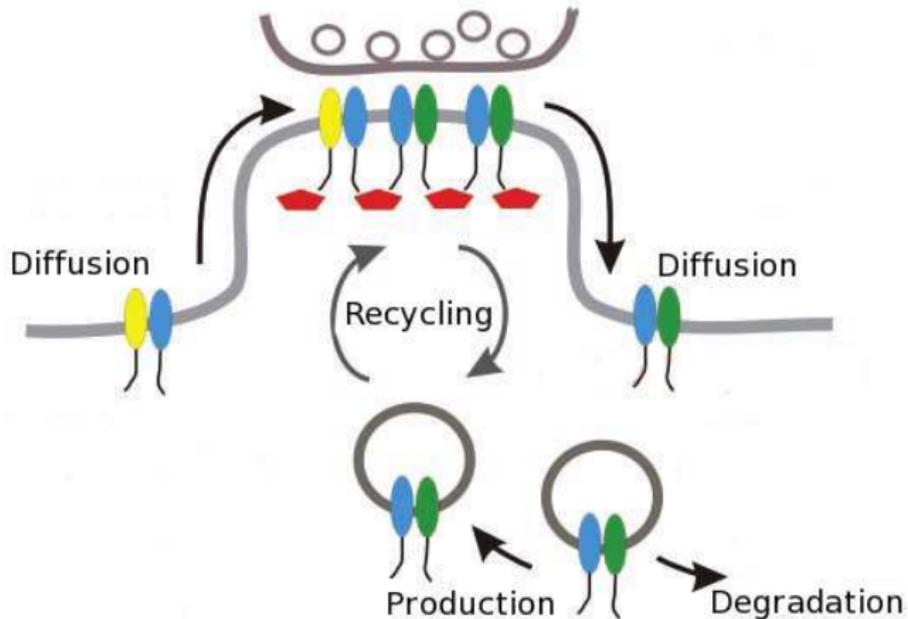


Synapses located in dendritic spines

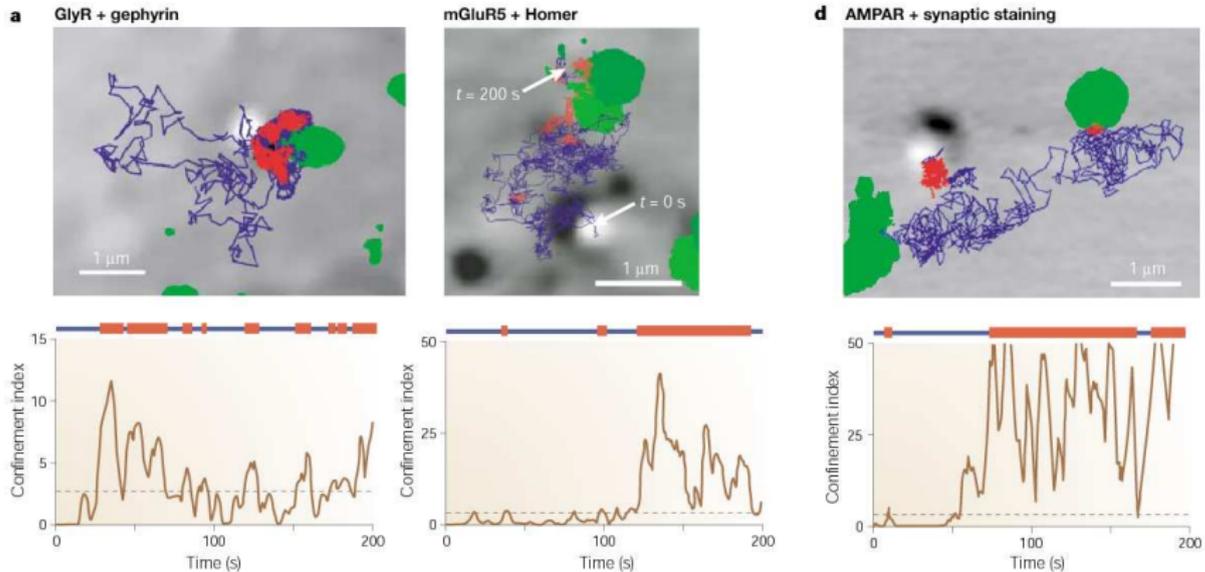


Matus, *Science* (2000)

Receptor trafficking at a synapse

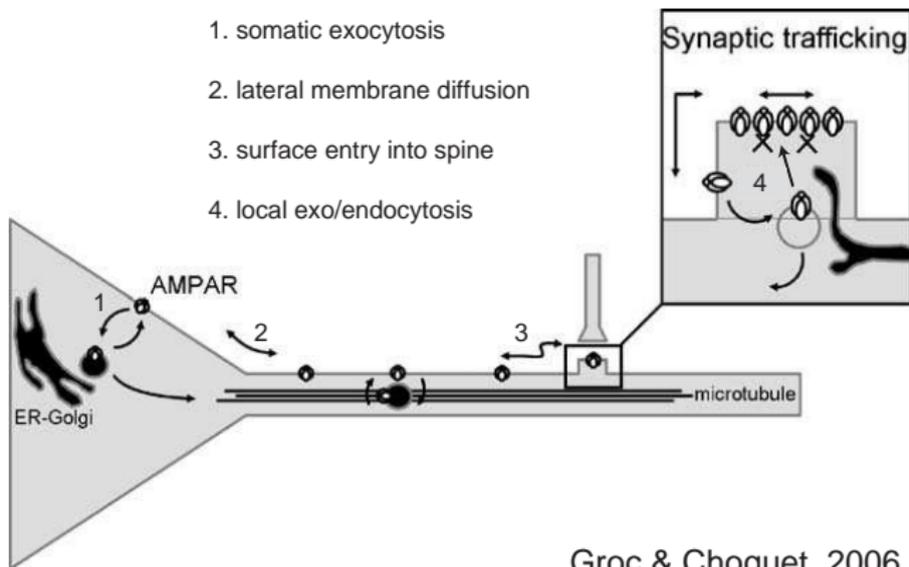


Receptors diffuse laterally between synapses



Triller & Choquet, *Nat. Rev. Neurosci.* (2003)

Long-range transport of receptors



- Single-spine model (deterministic)
- Single-synapse model (stochastic)
- 2D diffusion model
- 1D diffusion models
- Other diffusion-trapping problems

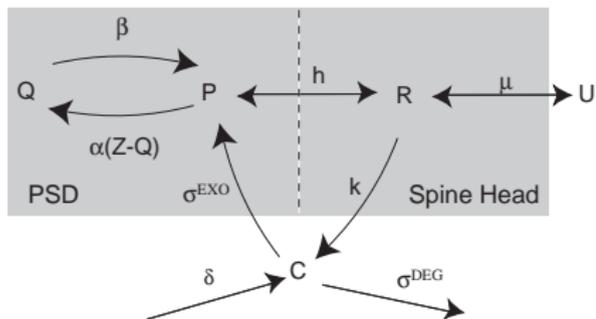
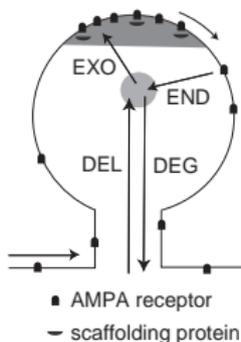
Model of single-spine AMPAR trafficking

Spine head:
$$\frac{dR}{dt} = \frac{1}{A} (\mu[U - R] - kR - h[R - P])$$

PSD unbound:
$$\frac{dP}{dt} = \frac{h}{a} [R - P] - \alpha[Z - Q]P + \beta Q + \frac{\sigma^{\text{EXO}} C}{a}$$

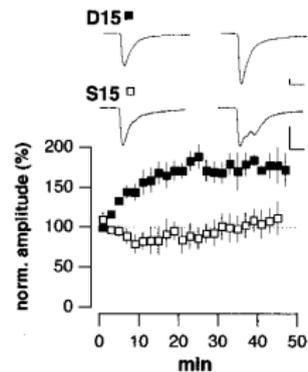
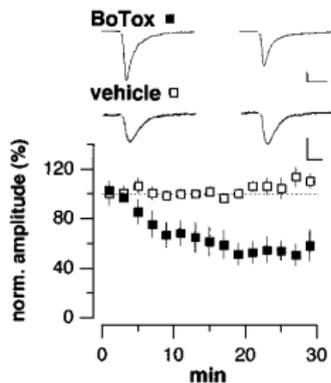
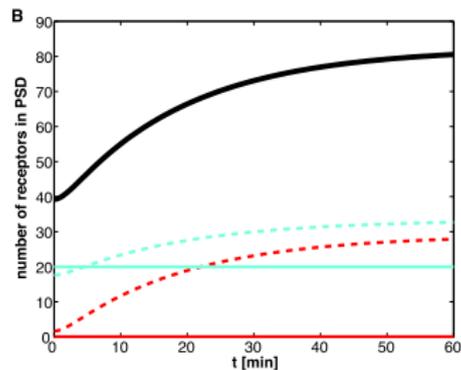
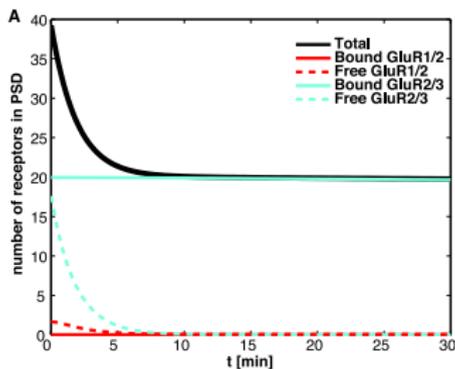
PSD bound:
$$\frac{dQ}{dt} = \alpha[Z - Q]P - \beta Q$$

Intracellular:
$$\frac{dC}{dt} = -\sigma^{\text{EXO}} C - \sigma^{\text{DEG}} C + kR + \delta$$



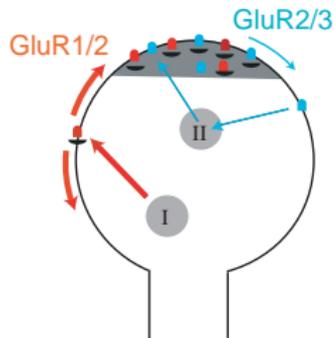
BAE & Bressloff, *J Neurosci* (2006)

Block exo/endocytosis

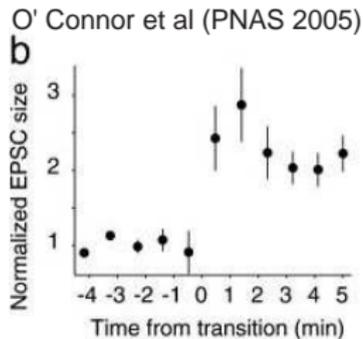
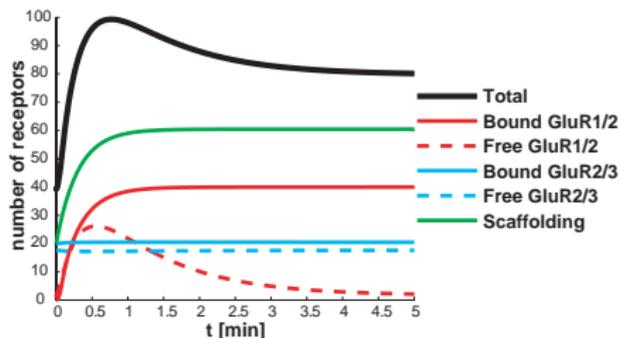


Luscher et al., *Neuron* (1999)

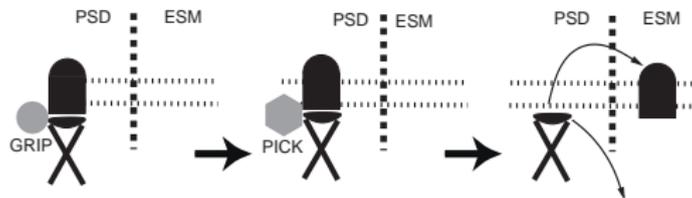
LTP simulation



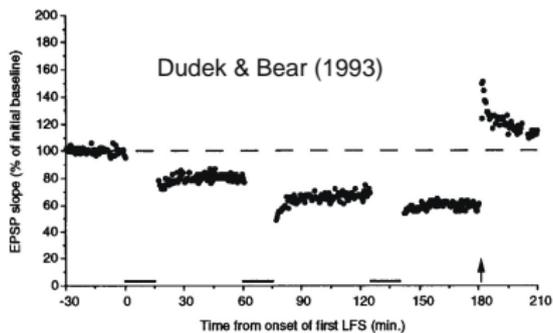
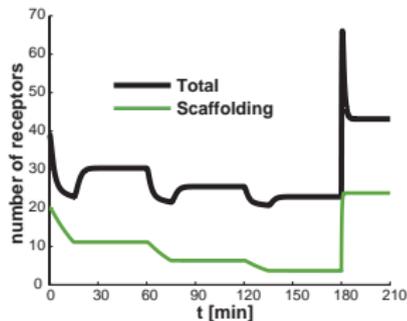
- Activation of GluR1/2 intracellular pool
- Rapid insertion of receptors into ESM
- AMPARs transport slot proteins into PSD



LTD simulation



- Switch from AMPA-GRIP to AMPA-PICK receptor-protein complexes
- Rapid unbinding from PSD and trafficking to ESM followed by endocytosis.
- Unbound scaffolding proteins are degraded.



Conclusions

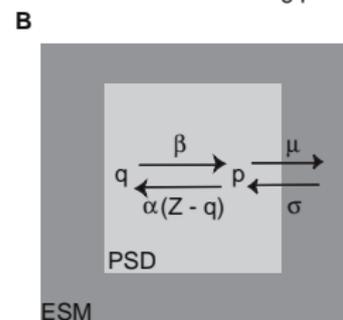
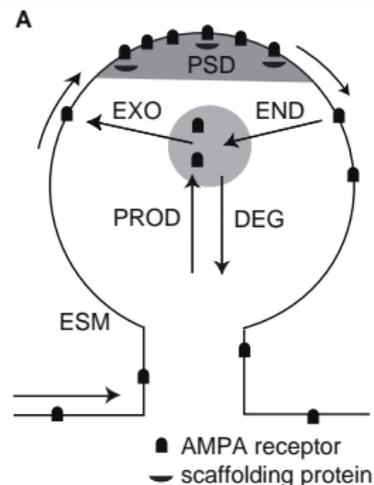
- ① Significant fraction of PSD receptors are **mobile** (Groc et al., 2004; Ashby et al., 2006)
 - Requires PSD-ESM barrier (Choquet & Triller, 2003)
- ② **Diffusive impedance** of spine neck is significant (Ashby et al., 2006)
- ③ Insertion of GluR1/2 during LTP must combine **synaptic targeting**
 - Requires increased hopping and binding rate (Schnell et al., 2002) and scaffolding (Shi et al., 2001)
- ④ Slow exchange of GluR1/2 with GluR2/3 after LTP requires **maintenance of additional binding sites** (McCormack et al., 2006)
- ⑤ LTD requires **loss of binding sites** (Colledge et al., 2003)

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Stochastic model of trafficking at PSD

$$\frac{dp}{dt} = -\alpha(Z - q)p + \beta q - \mu p + \sigma$$

$$\frac{dq}{dt} = \alpha(Z - q)p - \beta q$$

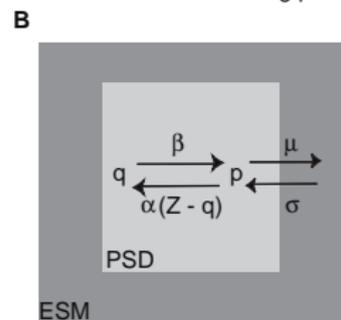
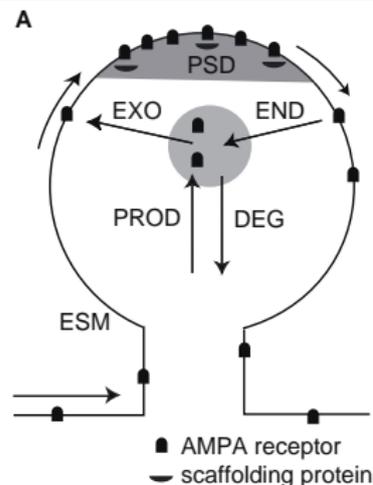


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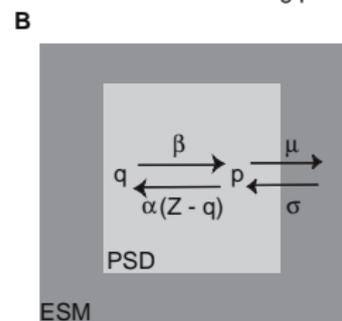
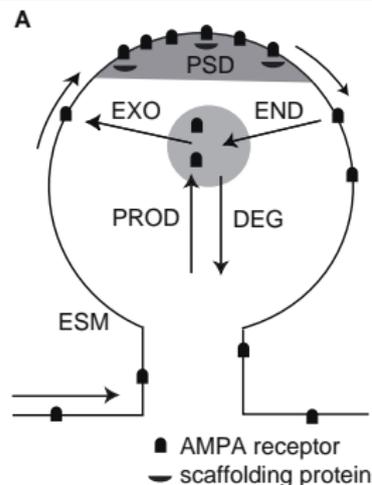
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$$\begin{aligned} \frac{dP_{n,m}}{dt} = & \sigma P_{n-1,m} + \mu(n+1)P_{n+1,m} \\ & + \alpha(n+1)[Z - (m-1)]P_{n+1,m-1} \\ & + \beta(m+1)P_{n-1,m+1} \\ & - [\sigma + \mu n + \alpha n(Z - m) + \beta m]P_{n,m} \end{aligned}$$



Stochastic model of trafficking at PSD

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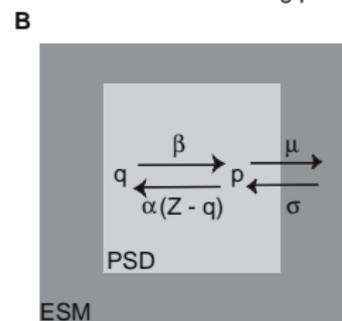
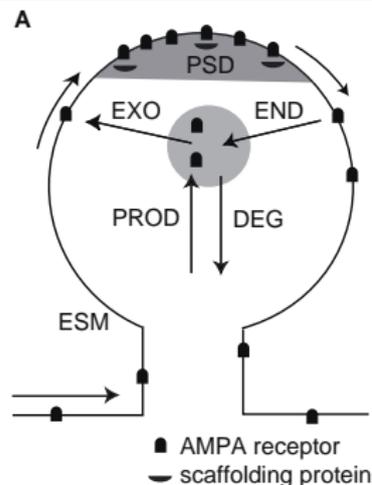
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$$\text{stochastic gate : } 0 < \mu_{open} \xrightleftharpoons[\gamma_+]{\gamma_-} \mu_{closed} = 0$$

$$\sigma(t) = C\mu(t) \quad (C \text{ bath conc.})$$



Analysis in two regimes: un/saturated binding sites

- Can do math in two regimes:
 - unsaturated binding sites: $m(t) \ll Z$ for all t (i.e., $\alpha n(t) \ll \beta$)
 - saturated binding sites: $m(t) = Z$ for all t (i.e., $\alpha n(t) \gg \beta$)

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- Unsaturated regime: master equation is linear in n, m
 - Generating function

$$G(u, v, t) = \sum_{n=0}^{\infty} \sum_{m=0}^{\infty} u^n v^m P_{n,m}(t)$$

satisfies first-order linear PDE

$$\frac{\partial G}{\partial t} + [\mu(t)(u-1) + \alpha Z(u-v)] \frac{\partial G}{\partial u} - \beta(u-v) \frac{\partial G}{\partial v} = \sigma(t)(u-1)G$$

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- Obtain mean, variance from derivatives of G

$$E_{\mu}(n) = \left. \frac{\partial G}{\partial u} \right|_{u=v=1}, \quad E_{\mu}(m) = \left. \frac{\partial G}{\partial v} \right|_{u=v=1}$$

Averaging over realizations of μ

- Can show that

$$E(n) \equiv \langle E_\mu(n) \rangle = C + (n_0 - C)\langle \mathcal{N}_{11} \rangle + (m_0 - C\alpha Z/\beta)\langle \mathcal{N}_{21} \rangle$$

$$E(m) \equiv \langle E_\mu(m) \rangle = C\alpha Z/\beta + (n_0 - C)\langle \mathcal{N}_{12} \rangle + (m_0 - C\alpha Z/\beta)\langle \mathcal{N}_{22} \rangle$$

where

$$\mathcal{N}(t) = \exp\left(-\int_0^t \mathcal{M}(t') dt'\right), \quad \mathcal{M}(t) = \begin{pmatrix} \mu(t) + \alpha Z & -\alpha Z \\ -\beta & \beta \end{pmatrix}$$

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- Can derive a system of ODEs for the averages of the entries of \mathcal{N} using method of Kubo and Zwanzig

Saturated binding sites

- Since $m(t) = Z$ for all t , master equation becomes

$$\frac{dP_n}{dt} = \mu(t) [CP_{n-1} + (n+1)P_{n+1}(t) - (C+n)P_n]$$

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- Brown et al. (*Biophys J*, 2000) showed that

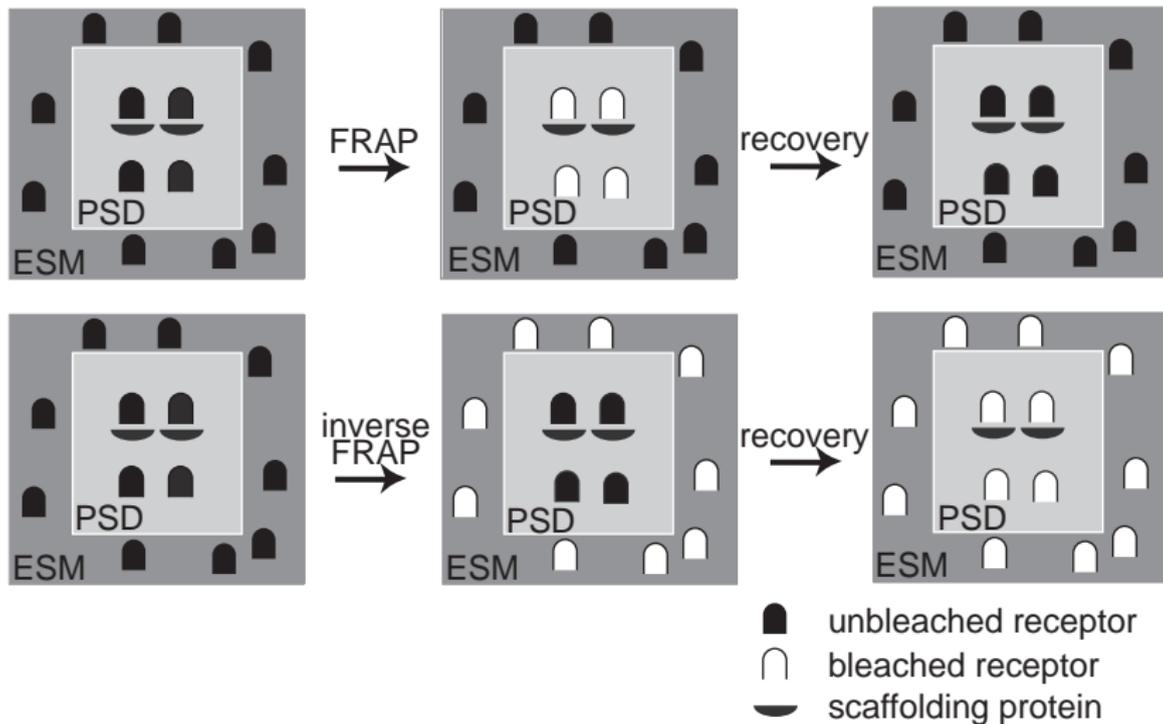
$$E(n) = (n_0 - C)\langle w \rangle + C$$

$$\text{Var}(n) = E(n) - n_0\langle w^2 \rangle + (n_0 - C)^2 (\langle w^2 \rangle - \langle w \rangle^2)$$

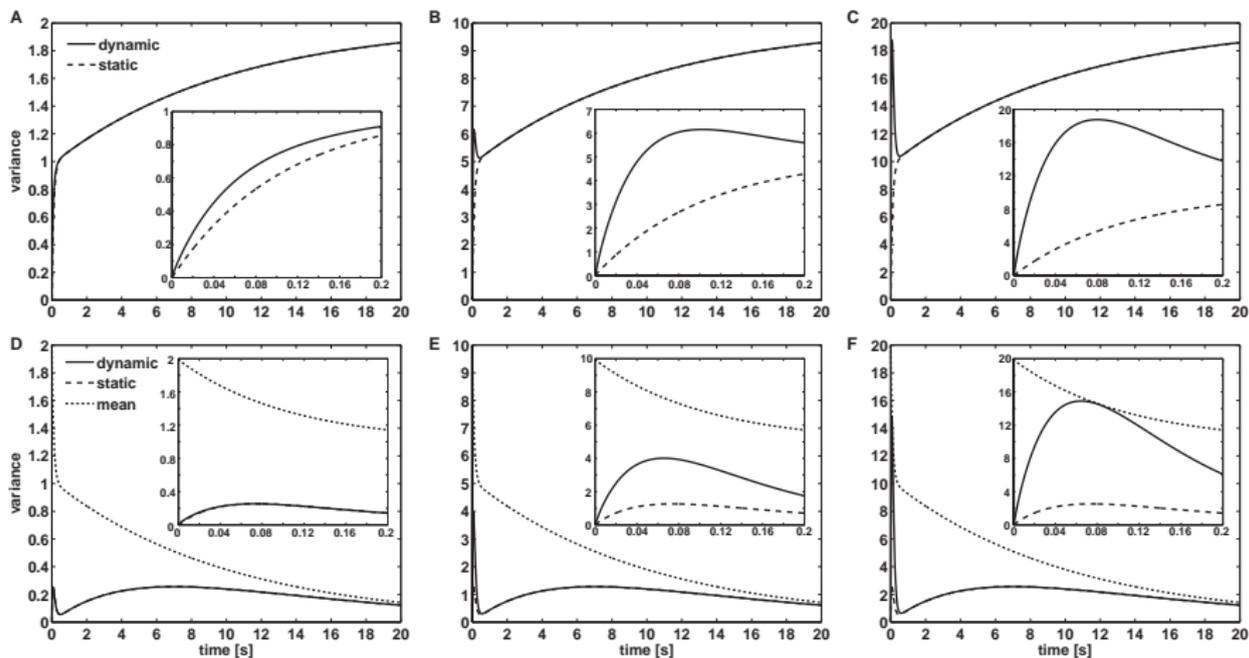
$$\langle w(t)^j \rangle = \begin{pmatrix} 1 \\ 1 \end{pmatrix}^T \exp \left[-t \begin{pmatrix} j\mu_o + \gamma_- & -\gamma_+ \\ -\gamma_- & \gamma_+ \end{pmatrix} \right] \begin{pmatrix} \Pi_o \\ \Pi_c \end{pmatrix}, \quad (j = 1, 2)$$

$$\Pi_o = \frac{\gamma_+}{\gamma_+ + \gamma_-}, \quad \Pi_c = \frac{\gamma_-}{\gamma_+ + \gamma_-}$$

FRAP and inverse FRAP experiments

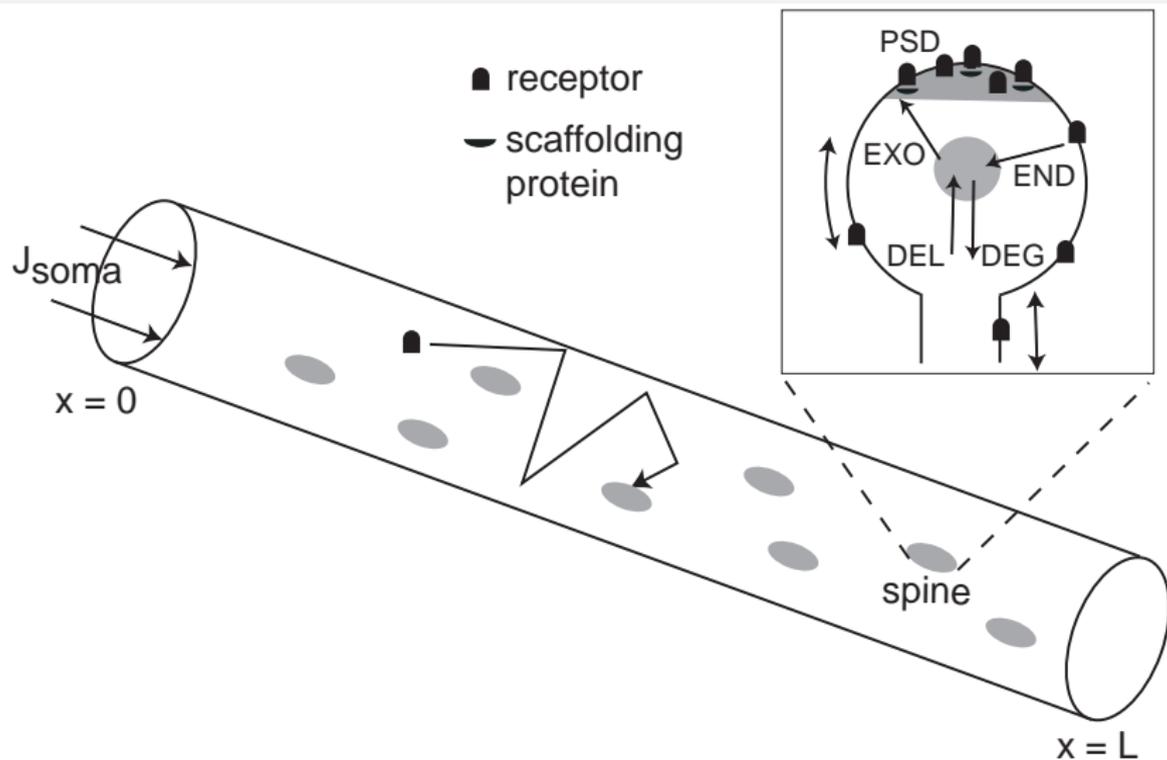


Simulations of FRAP and inverse FRAP



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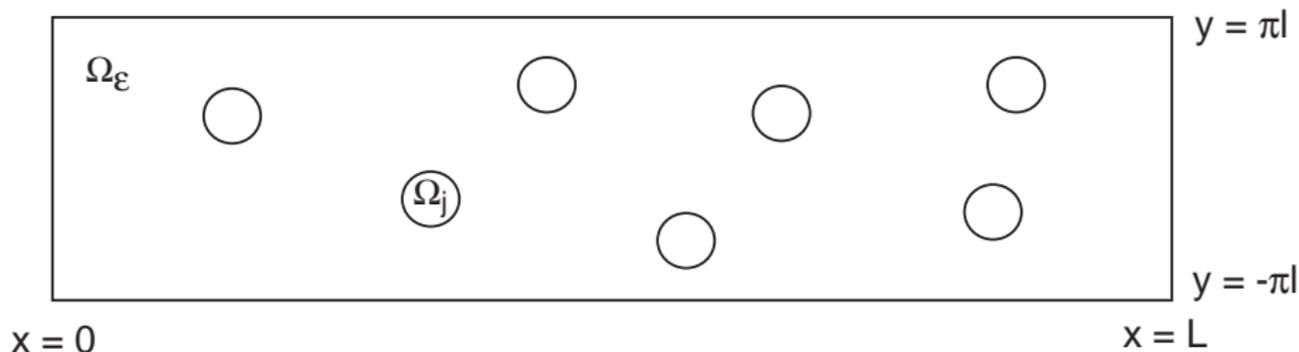
Treat dendritic membrane as cylinder with holes



Bressloff, BAE & Ward, *SIAM J Appl Math* (2008)

Diffusion equation on dendritic membrane

$$\frac{\partial U}{\partial t} = D \nabla^2 U \quad \text{on } \Omega_\varepsilon$$



- U = receptor concentration
- Ω_ε is rectangle $(0, L) \times (-\pi l, \pi l)$ minus the holes

$$\Omega_j = \{\mathbf{r} \in \Omega_0 \mid |\mathbf{r} - \mathbf{r}_j| \leq \varepsilon \rho\}, \quad j = 1, \dots, N$$

Boundary conditions

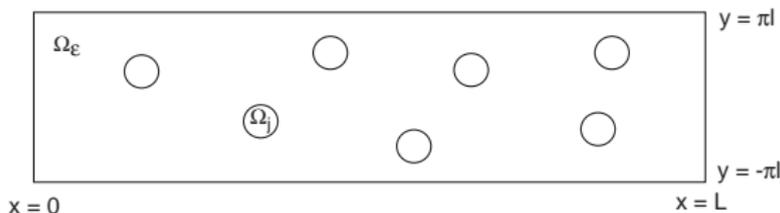
- Periodic bcs at $y = \pm\pi l$
- No-flux bc at $x = L$, and at $x = 0$

$$-D \frac{\partial U}{\partial x} = J_{soma} = \frac{\sigma}{2\pi l}$$

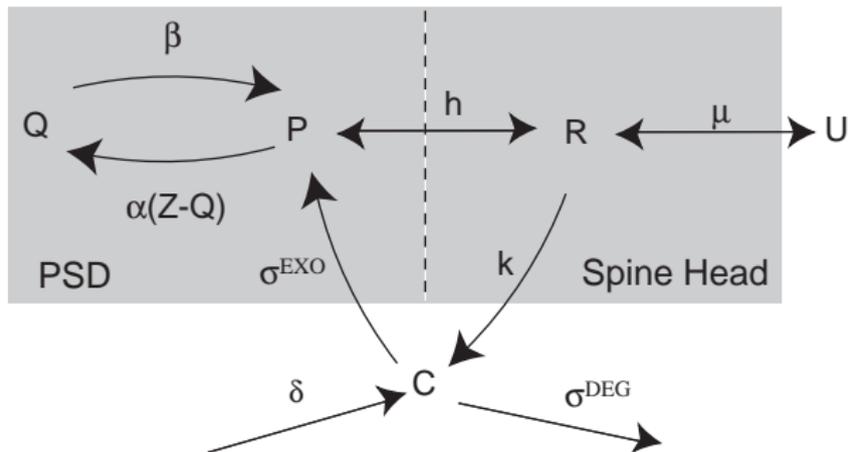
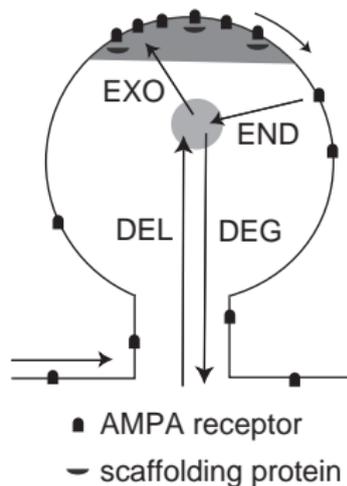
- bcs at the holes:

$$-D \frac{\partial U}{\partial \mathbf{n}}(\mathbf{r}, t) = \frac{\mu_j}{2\pi\epsilon\rho} (U(\mathbf{r}, t) - R_j), \quad \mathbf{r} \in \partial\Omega_j$$

- μ_j = spine neck hopping rate
- R_j = receptor concentration on surface of j th spine



Treat each spine as before



Steady-state solution

- Assume concentrations in j th spine see mean value of U on $\partial\Omega_j$:

$$U_j = \frac{1}{2\pi\epsilon\rho} \int_{\partial\Omega_j} U(\mathbf{r}) d\mathbf{r}$$

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- U_j 's are determined by solving $\nabla^2 U = 0$ in Ω_ε with boundary conditions
- But this is **hard** because of boundary conditions at the holes!

$$-\varepsilon D \frac{\partial U}{\partial \mathbf{n}}(\mathbf{r}) = \frac{\mu_j}{2\pi\rho} (U(\mathbf{r}) - R_j), \quad \mathbf{r} \in \partial\Omega_j$$

Three steps for finding approximate steady-state solution

- 1 Solve assuming $U = U_j$ on the boundary of j th hole

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 - **Singular perturbation:** match logarithmic solutions in each inner region

$$|\mathbf{r} - \mathbf{r}_j| = \mathcal{O}(\varepsilon)$$

with Green's function singularities in outer region

$$|\mathbf{r} - \mathbf{r}_j| = \mathcal{O}(1) \text{ for all } j$$

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$$-\varepsilon D \frac{\partial U}{\partial \mathbf{n}}(\mathbf{r}) = \frac{\hat{\mu}_j}{2\pi\rho} (U_j - \hat{R}_j), \quad \mathbf{r} \in \partial\Omega_j$$

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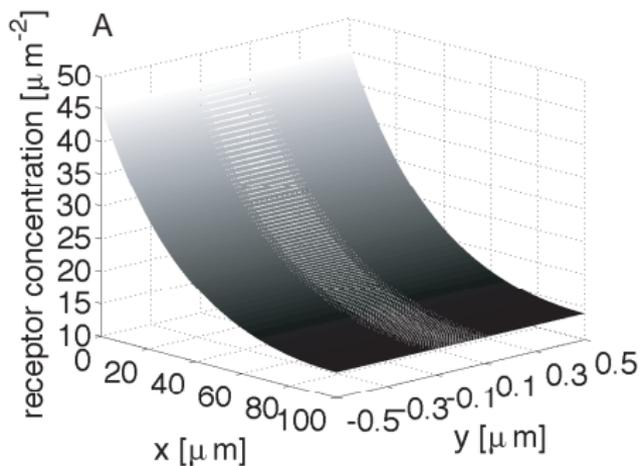
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- 3 Conservation condition gives $(N + 1)$ th equation

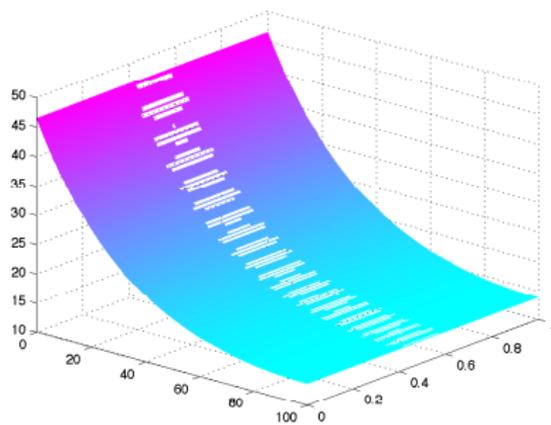
$$\sigma = \sum \hat{\mu}_j (U_j - \hat{R}_j)$$

Comparison of dendritic receptor concentration

perturbation solution



numerical solution



- Dendrite $100\mu\text{m}$ long, circumference $1\mu\text{m}$, $\epsilon\rho = 0.1\mu\text{m}$
- 100 identical spines spaced $1\mu\text{m}$ apart, all in a row
- Solutions are almost identical!
- Similar results if spines are not identical, not in a row

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2D model well-approximated by 1D model

When the aspect ratio $L/l \gg 1$, we can approximate 2D model by the following 1D model

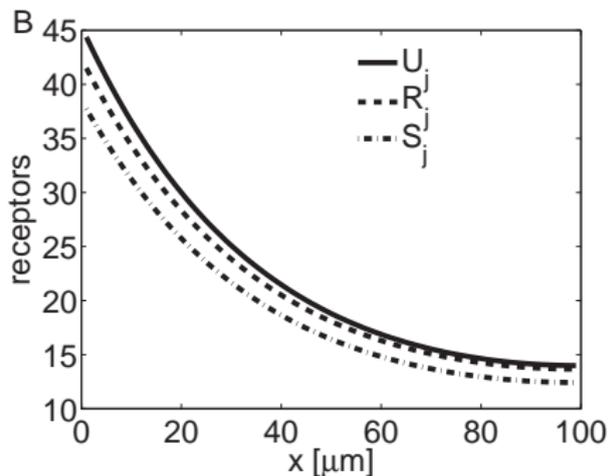
$$\frac{\partial U}{\partial t} = D \frac{\partial^2 U}{\partial x^2} - \sum_{j=1}^N \delta(x - x_j) \mu_j (U_j - R_j)$$

$$-D \left. \frac{\partial U}{\partial x} \right|_{x=0} = J_{\text{soma}}, \quad \left. \frac{\partial U}{\partial x} \right|_{x=L} = 0.$$

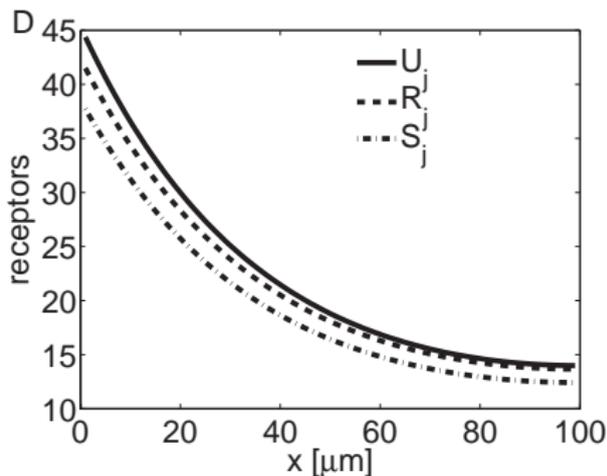
Bressloff & BAE, *PRE* (2007)

Comparison of models

2D model



1D model



- 2D model as before
 - Dendrite $100\mu\text{m}$ long, circumference $1\mu\text{m}$, $\epsilon\rho = 0.1\mu\text{m}$
 - 100 identical spines spaced $1\mu\text{m}$ apart, all in a row
- 1D model use same parameters when relevant
- Solutions are almost identical!

Can we make things even simpler?

Treat spine population as continuous density

If spines are sufficiently dense, treat sum of delta functions as a density η

$$\frac{\partial U}{\partial t} = D \frac{\partial^2 U}{\partial x^2} - \eta(x)\mu(x)(U - R)$$
$$-D \left. \frac{\partial U}{\partial x} \right|_{x=0} = J_{\text{soma}}, \quad \left. \frac{\partial U}{\partial x} \right|_{x=L} = 0.$$

BAE & Bressloff, *J Comput Neurosci* (2008)

Steady-state solution for identical spines: “cable” equation

- Assume all parameters are x -independent, then get “cable” equation for receptor trafficking

$$\frac{d^2 U}{dx^2} - \Lambda^2 U = -\Lambda^2 \hat{R}$$

$$\Lambda = \sqrt{\frac{\eta \hat{\mu}}{D}} \text{ is length-scale of diffusive coupling}$$

Steady-state solution for identical spines: “cable” equation

- Assume all parameters are x -independent, then get “cable” equation for receptor trafficking

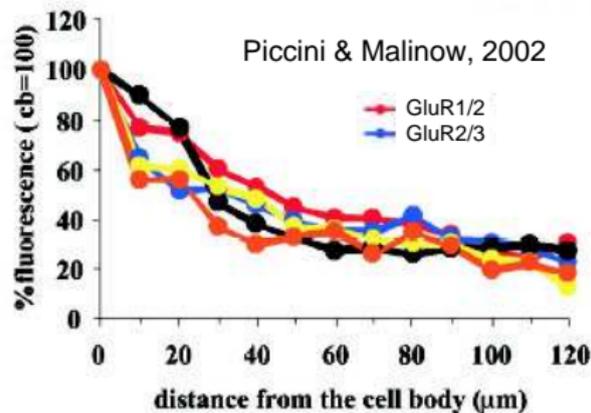
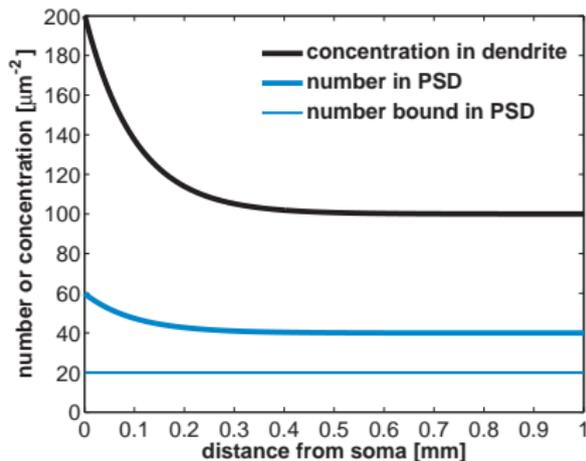
$$\frac{d^2 U}{dx^2} - \Lambda^2 U = -\Lambda^2 \widehat{R}$$

$$\Lambda = \sqrt{\frac{\eta \widehat{\mu}}{D}} \text{ is length-scale of diffusive coupling}$$

- Solve using Green’s function methods

$$U(x) = \frac{J_{\text{soma}}}{D} \frac{\cosh(\Lambda(x - L))}{\Lambda \sinh(\Lambda L)} + \widehat{R}$$

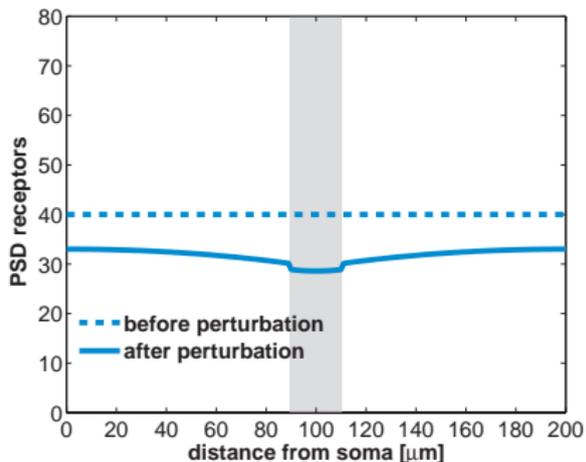
Steady-state receptor concentrations for identical spines



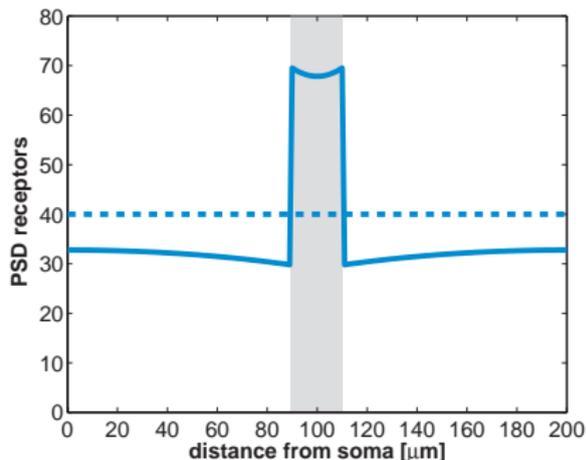
- Dendrite 1 mm long
- 1,000 identical spines spaced $1\mu\text{m}$ apart
- Two sources of receptors
 - at soma
 - local intracellular delivery

Consequences of diffusive coupling

10-fold reduction in
rate of exocytosis
in gray region

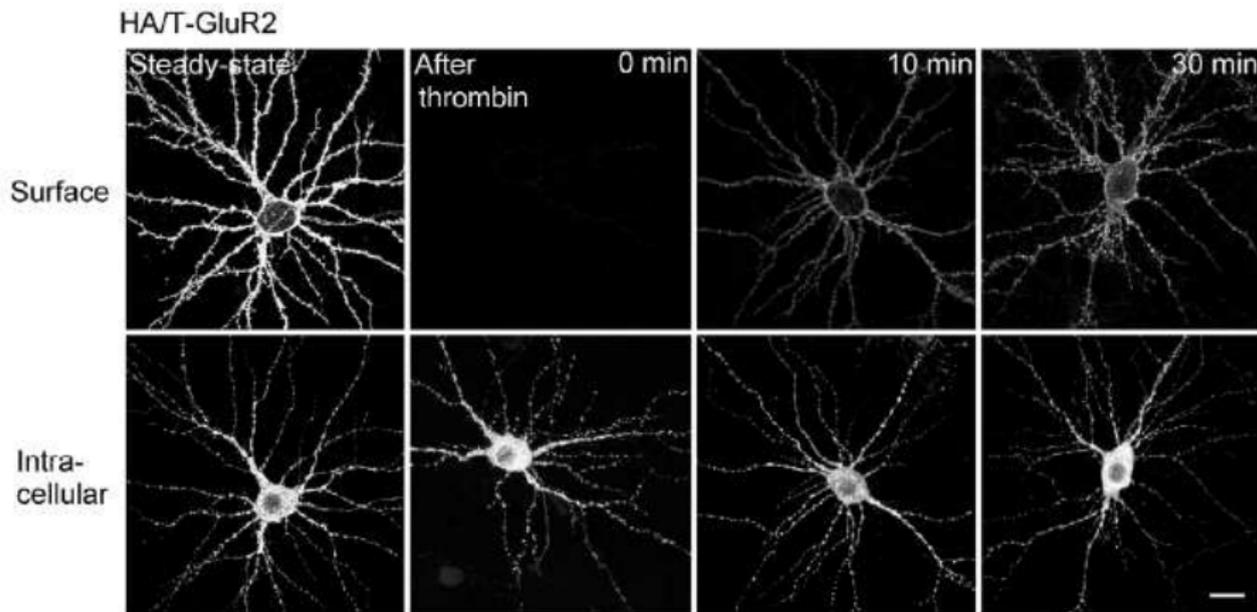


10-fold increase in
rate of endocytosis
in gray region



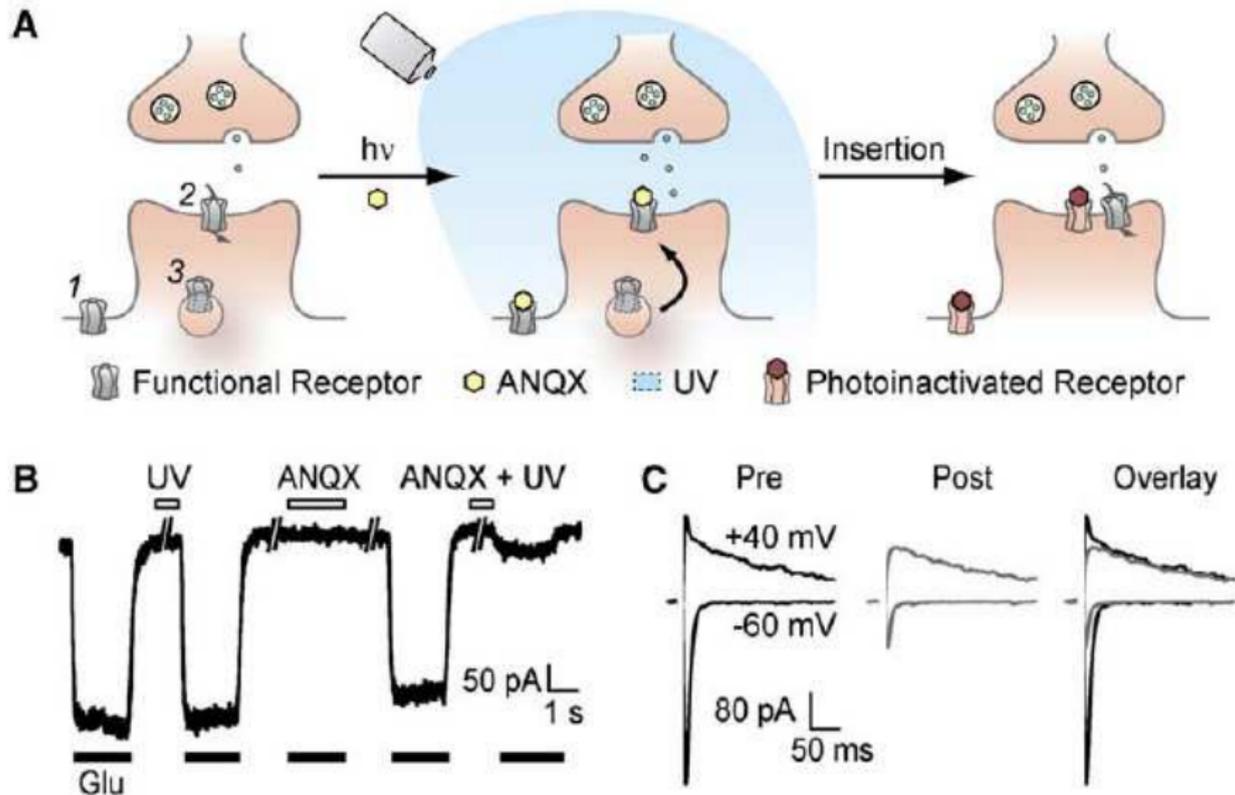
Steady-state is nice...
...but what about time-dependent phenomena?

AMPA receptor recycling via thrombin cleavage



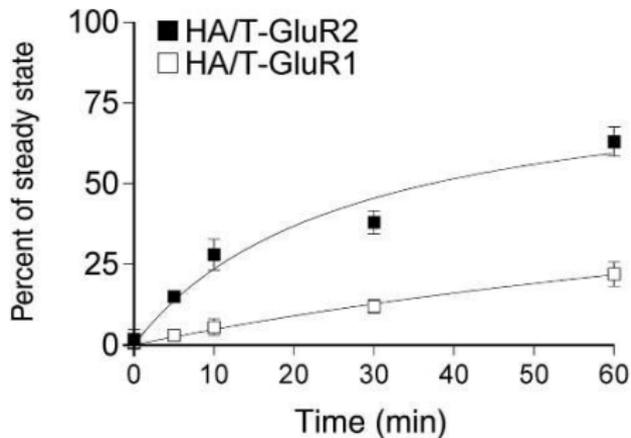
Passafaro et al., *Nat. Neurosci.* (2001)

AMPA receptor recycling via photoinactivation

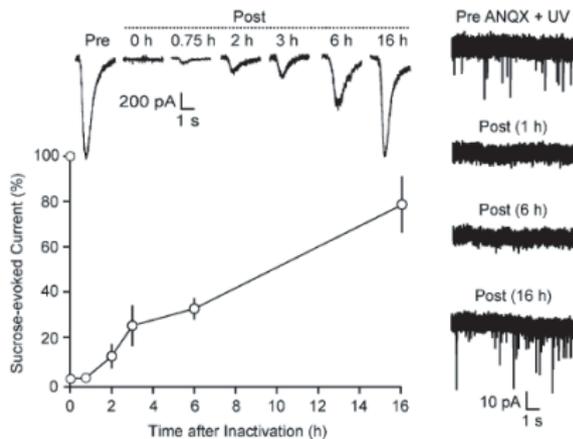


Fast or slow recycling of AMPA receptors?

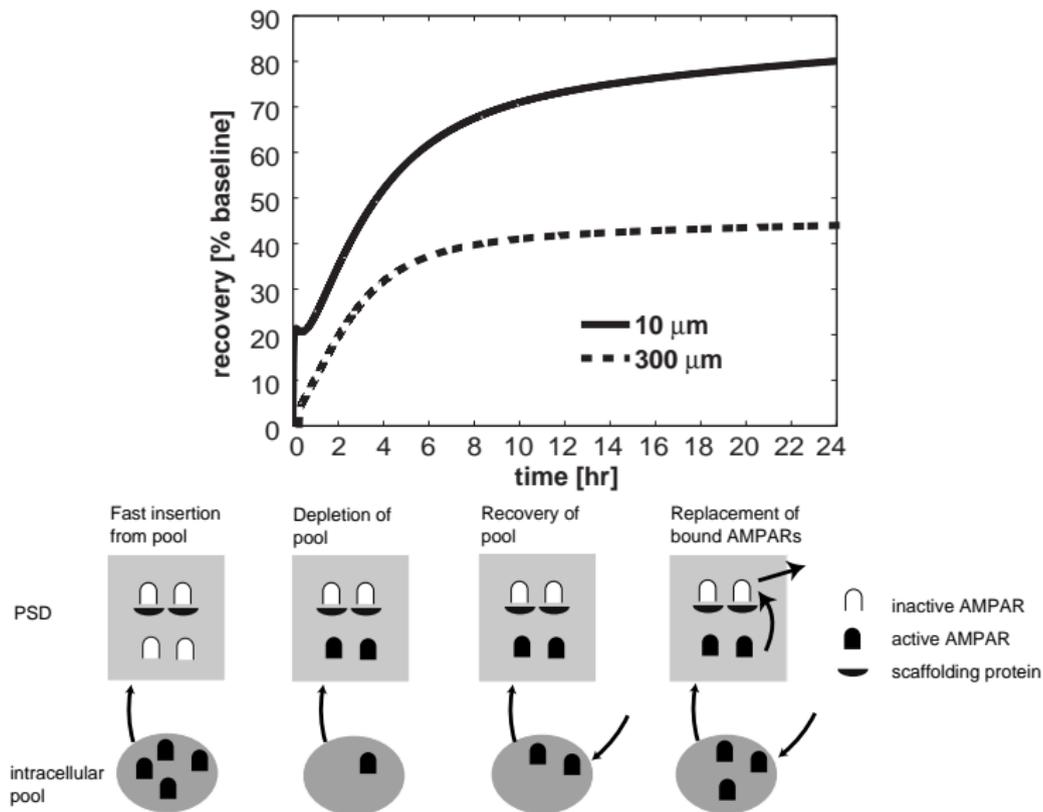
Passafaro et al., 2001



Adesnik et al., 2005

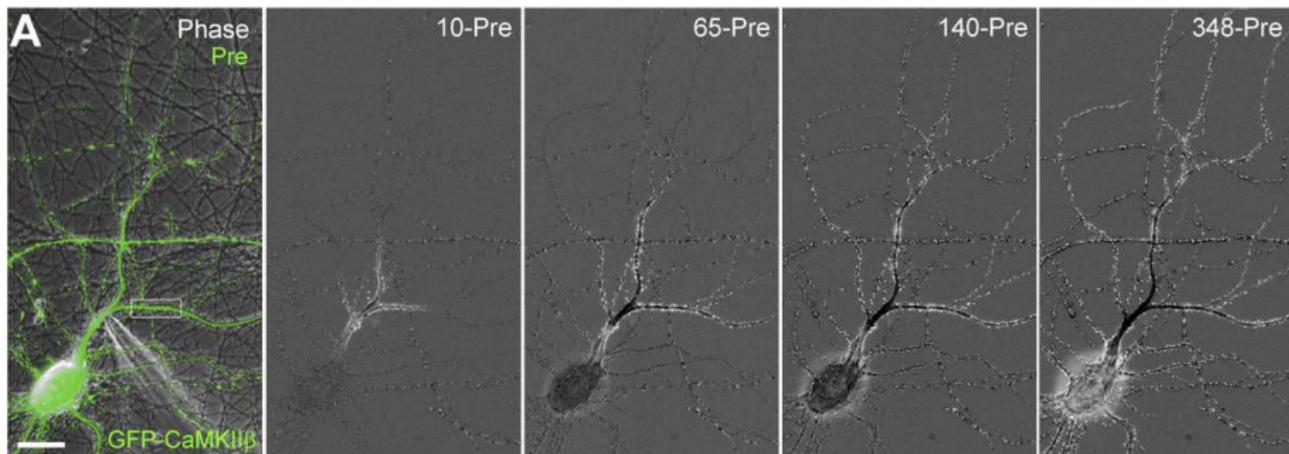


Simulation of photoinactivation of AMPA receptors



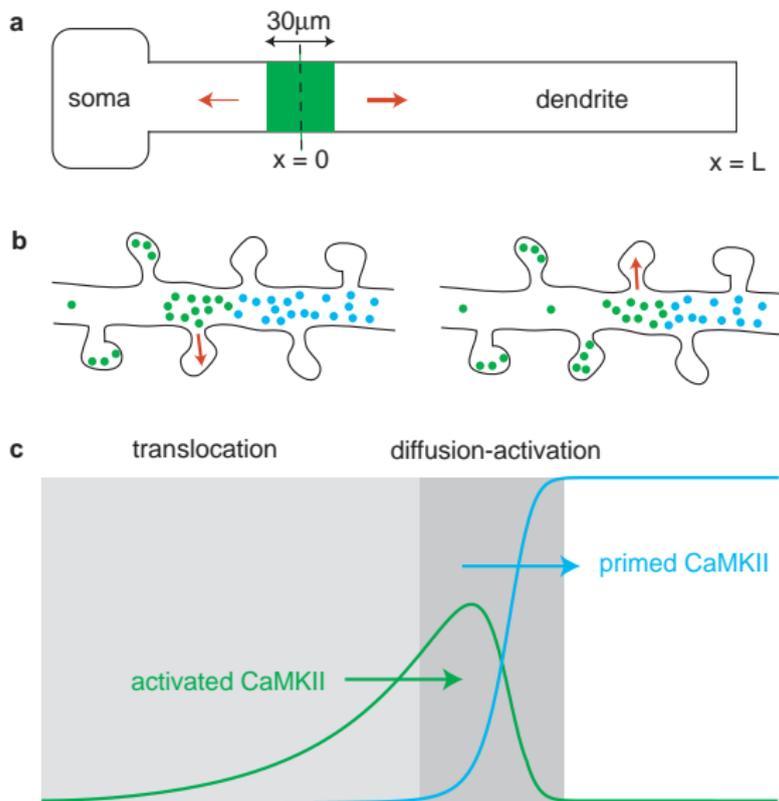
- Single-spine model (deterministic)
- Single-synapse model (stochastic)
- 2D diffusion model
- 1D diffusion models
- Other diffusion-trapping problems

CaMKII translocation waves



Rose et al., *Neuron* (2009)

Diffusion-activation model of CaMKII translocation waves



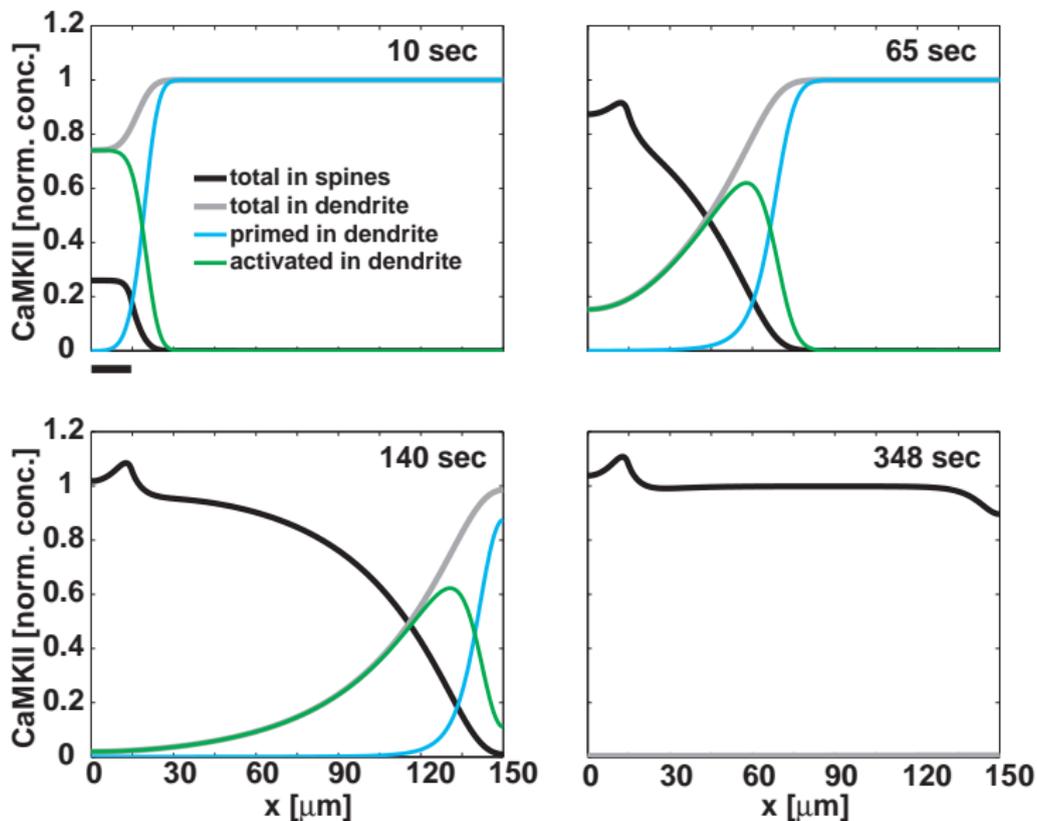
Equations for diffusion-activation model

$$\begin{aligned}\frac{\partial p}{\partial t} &= D \frac{\partial^2 p}{\partial x^2} - kap \\ \frac{\partial a}{\partial t} &= D \frac{\partial^2 a}{\partial x^2} + kap - ha \\ \frac{\partial s}{\partial t} &= ha\end{aligned}$$

- p = concentration of primed CaMKII in shaft
- a = concentration of activated CaMKII in shaft
- s = concentration of activated CaMKII in spines
- k, h = rate of activation, translocation

BAE & Bressloff, *In prep.*

Simulation of diffusion-activation model



Calculation of wave speed

- When $h = 0$ (no translocation), recover Fisher's equation with speed

$$c = 2\sqrt{Dk}$$

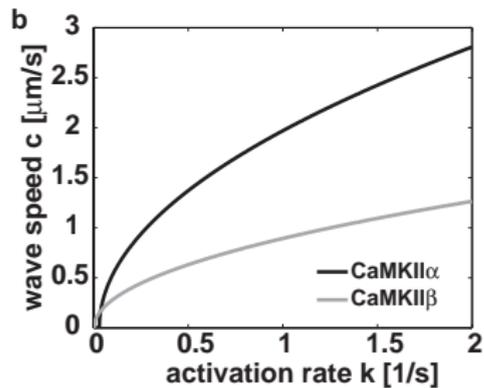
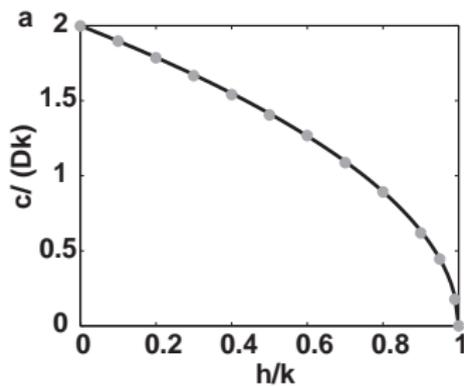
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- When $h = 0$ (no translocation), recover Fisher's equation with speed

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- When $h \neq 0$, wave speed is

$$c = 2\sqrt{D(k - h)}$$



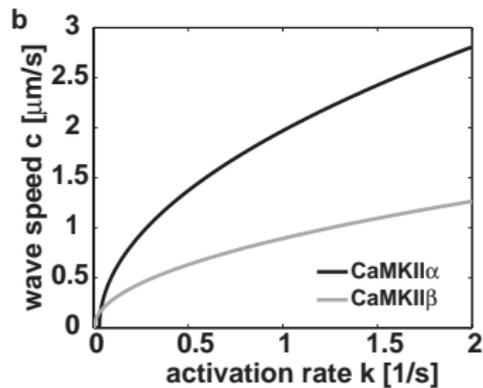
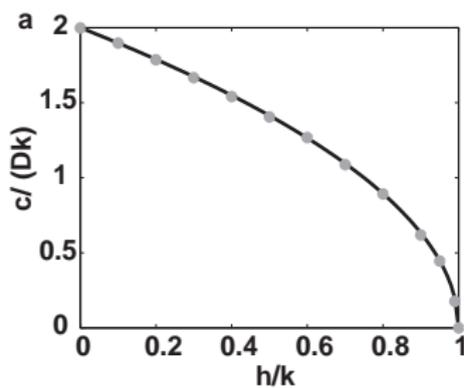
Calculation of wave speed

- When $h = 0$ (no translocation), recover Fisher's equation with speed

$$c = 2\sqrt{Dk}$$

- When $h \neq 0$, wave speed is

$$c = 2\sqrt{D(k - h)}$$



- Wave propagation failure when $k < h$

Other projects with diffusion-trapping models

- other heterosynaptic molecules, e.g. PSD-95
- changes in spine volume during late-phase LTP
 - mRNA transport/capture/translation
 - F-actin regulation/stabilization by AMPA receptors
- protein transport/capture during synaptogenesis, e.g. NMDA receptors
- AMPA receptor trafficking in more detailed model of PSD
- put all the pieces together!

Thank you!

Thanks to

- Paul Bressloff (Utah)
- Michael Ward (UBC)
- NSF

